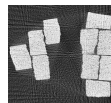
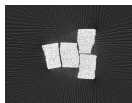
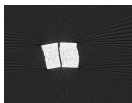
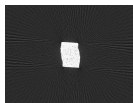
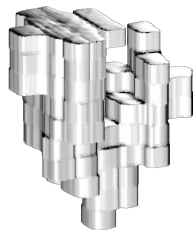
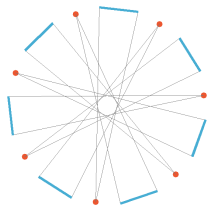


# X-ray tomography

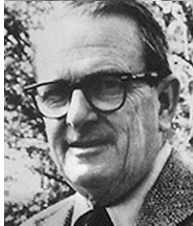
**Samuli Siltanen**

Department of Mathematics and Statistics  
University of Helsinki, Finland  
[samuli.siltanen@helsinki.fi](mailto:samuli.siltanen@helsinki.fi)  
<http://www.siltanen-research.net>

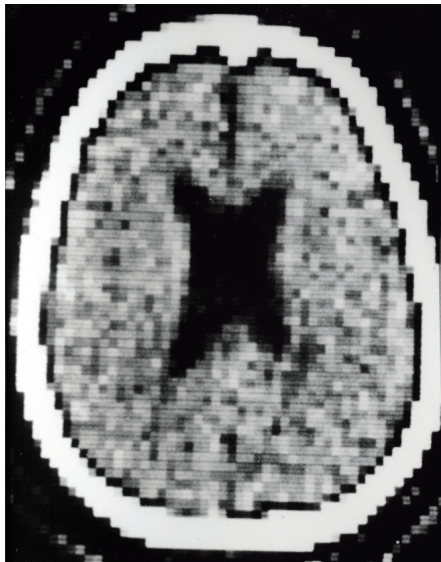
November 28, 2014



# Godfrey Hounsfield and Allan McLeod Cormack were the first to develop X-ray tomography



Cormack (left) and Hounsfield (top) received Nobel prizes in 1979. Right: an early tomographic image.



# Reconstruction of a function from its line integrals was first invented by Johann Radon in 1917



This is Radon's original formula:

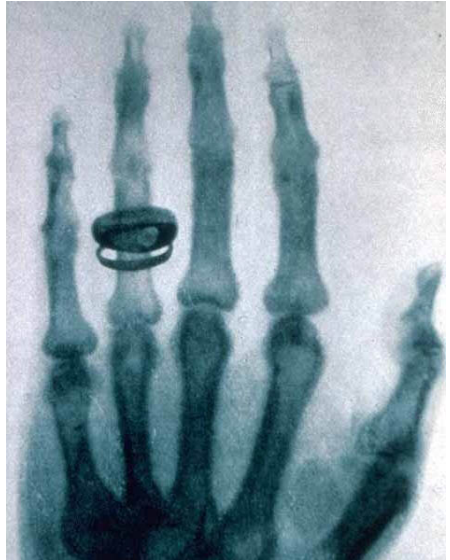
$$f(P) = -\frac{1}{\pi} \int_0^\infty \frac{d\overline{F}_P(q)}{q}.$$

Almost all tomography devices use *Filtered Back-Projection* (FBP), an algorithm derived from the above formula. See [Natterer 1986].

We consider sparsely sampled data. FBP is not optimal for such data, and we need to use for example Total Variation (TV) regularization:

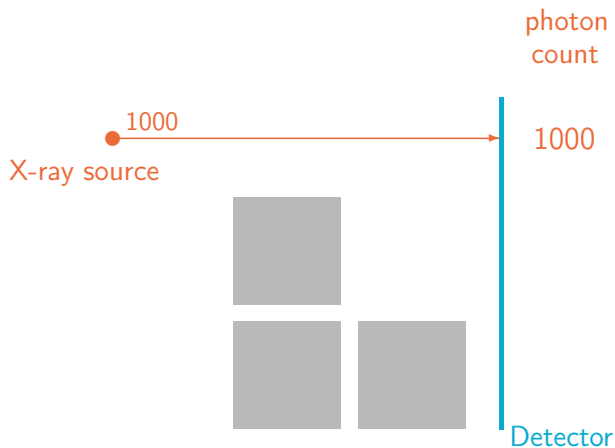
$$\text{minimize}\{\|\mathbf{A}f - \mathbf{m}\|_2^2 + \alpha\|\nabla f\|_1\}.$$

**Wilhelm Conrad Röntgen invented X-rays and was awarded the first Nobel Prize in Physics in 1901**

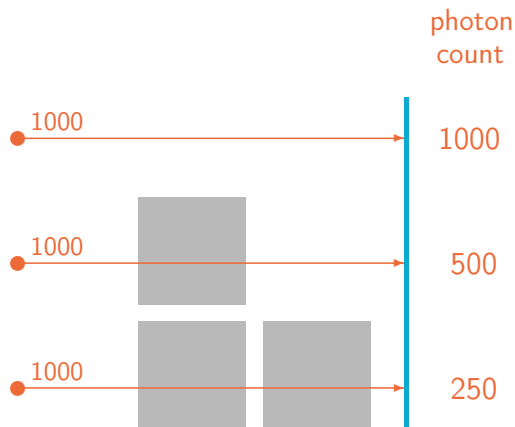




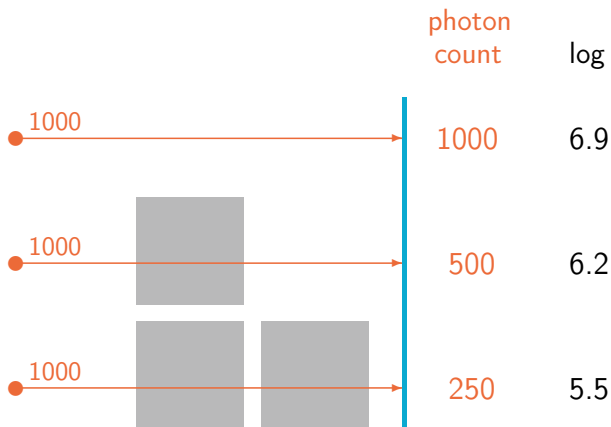
A digital X-ray detector counts how many photons arrive at each pixel



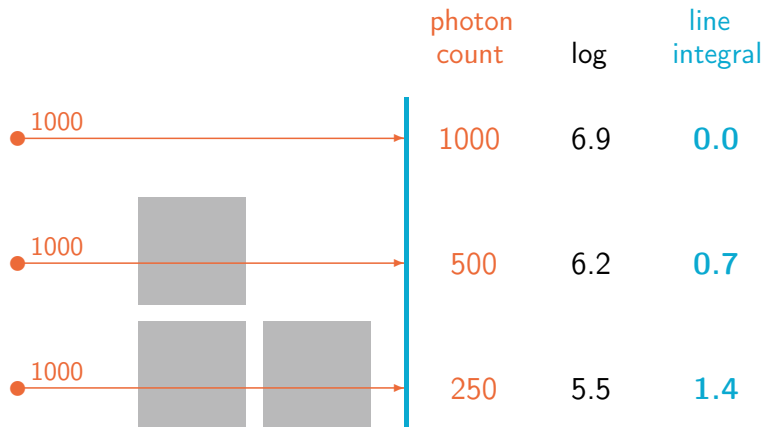
# Adding material between the source and detector reveals the exponential X-ray attenuation law



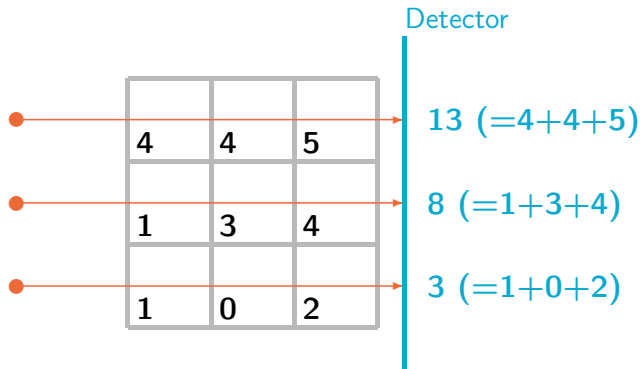
We take logarithm of the photon counts to compensate for the exponential attenuation law



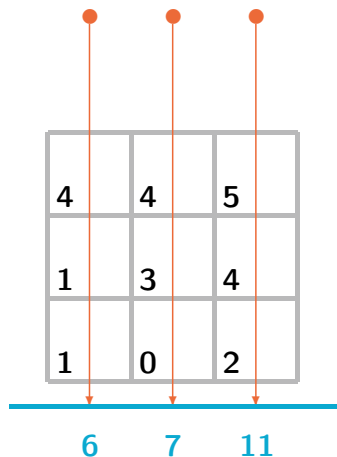
Final calibration step is to subtract the logarithms from the empty space value (here 6.9)



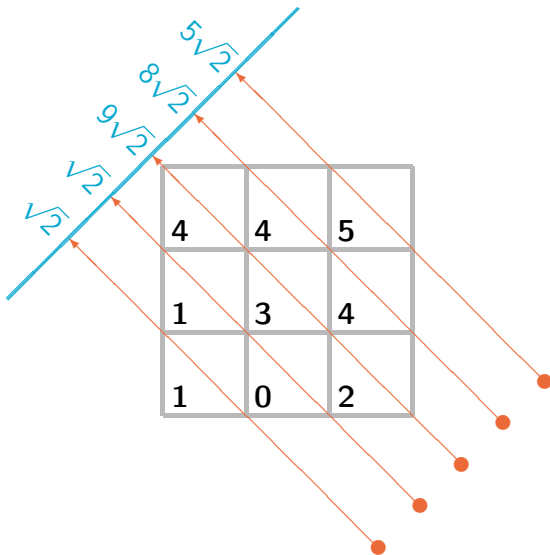
A projection image is produced by parallel X-rays and several detector pixels (here three pixels)



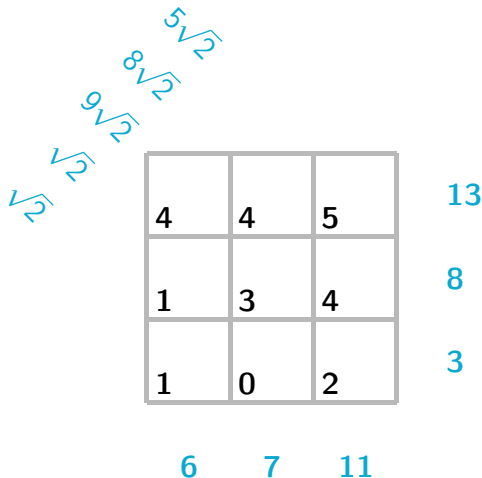
For tomographic imaging it is essential to record projection images from different directions



The length of X-rays traveling inside each pixel is important, thus here the square roots

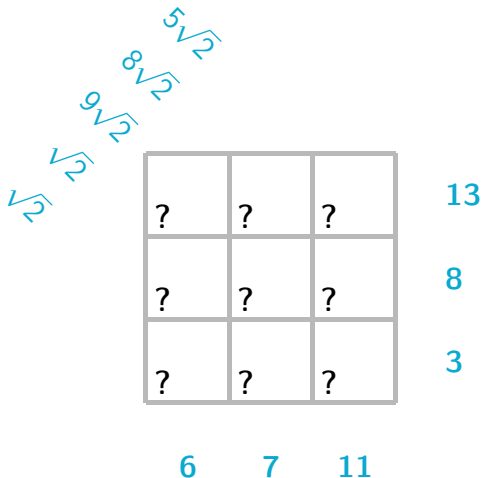


The direct problem of tomography is to find the projection images from known tissue

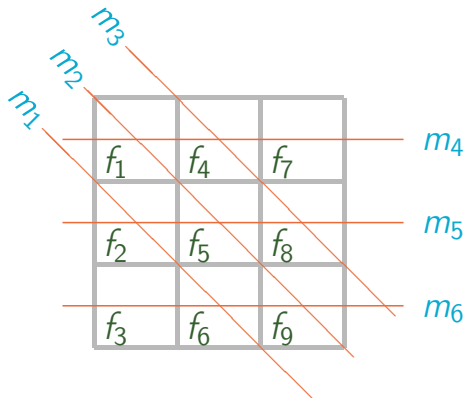




The inverse problem of tomography is to reconstruct the interior from X-ray data



We write the reconstruction problem in matrix form

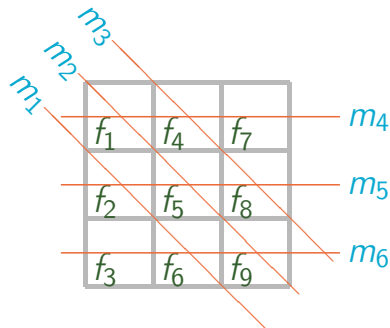


$$f = \begin{bmatrix} f_1 \\ f_2 \\ f_3 \\ f_4 \\ f_5 \\ f_6 \\ f_7 \\ f_8 \\ f_9 \end{bmatrix}, \quad m = \begin{bmatrix} m_1 \\ m_2 \\ m_3 \\ m_4 \\ m_5 \\ m_6 \end{bmatrix},$$

Measurement model:  $m = Af + \varepsilon$

This is the matrix equation related to the above measurement

$$\begin{bmatrix} m_1 \\ m_2 \\ m_3 \\ m_4 \\ m_5 \\ m_6 \end{bmatrix} = \begin{bmatrix} 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 \\ \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} \\ 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 \\ 1 & 0 & 0 & 1 & 0 & 0 & 1 & 0 & 0 \\ 0 & 1 & 0 & 0 & 1 & 0 & 0 & 1 & 0 \\ 0 & 0 & 1 & 0 & 0 & 1 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} f_1 \\ f_2 \\ f_3 \\ f_4 \\ f_5 \\ f_6 \\ f_7 \\ f_8 \\ f_9 \end{bmatrix} + \begin{bmatrix} \varepsilon_1 \\ \varepsilon_2 \\ \varepsilon_3 \\ \varepsilon_4 \\ \varepsilon_5 \\ \varepsilon_6 \end{bmatrix}$$



# The VT device was developed in 2001–2012 by

Nuutti Hyvönen

Seppo Järvenpää

Jari Kaipio

Martti Kalke

Petri Koistinen

Ville Kolehmainen

Matti Lassas

Jan Moberg

Kati Niinimäki

Juha Pirttilä

Maaria Rantala

Eero Saksman

Henri Setälä

Erkki Somersalo

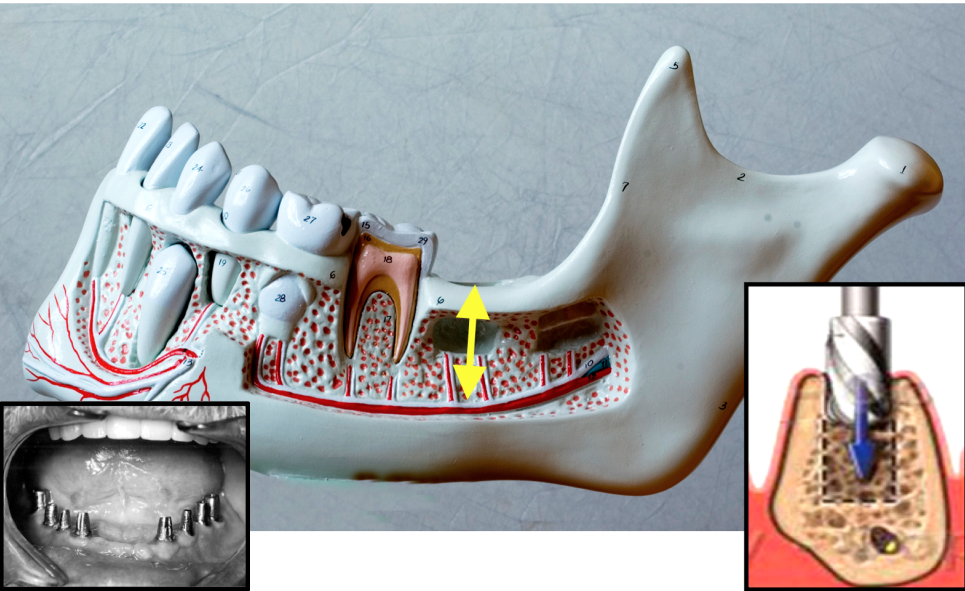
Antti Vanne

Simopekka Vänskä

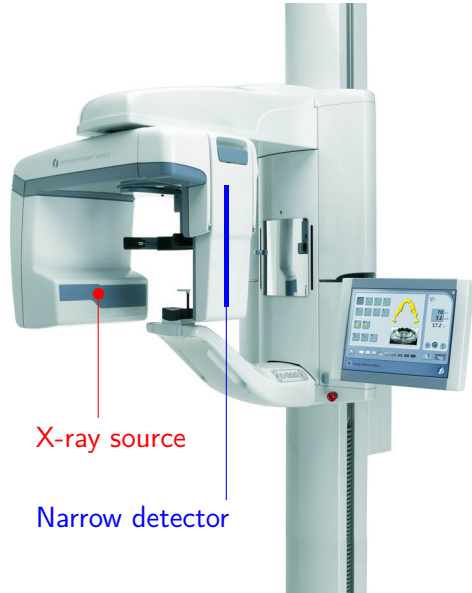
Richard L. Webber



**Application: dental implant planning, where a missing tooth is replaced with an implant**



Nowadays, a digital panoramic imaging device is standard equipment at dental clinics



A panoramic dental image offers a general overview showing all teeth and other dento-maxillofacial structures simultaneously.

Panoramic images are not suitable for dental implant planning because of unavoidable geometric distortion.

**We reprogram the panoramic X-ray device so that it collects projection data by scanning**

(Loading video)

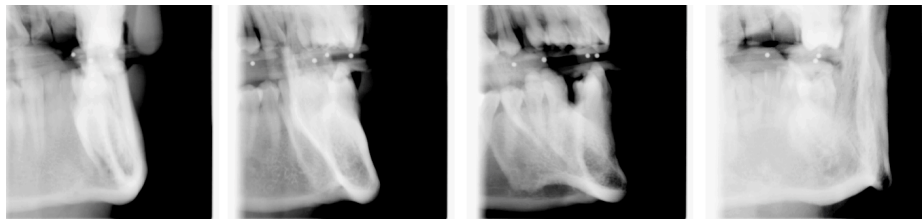
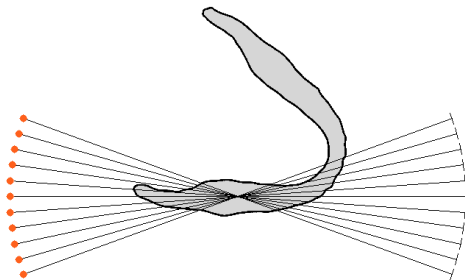
We reprogram the panoramic X-ray device so that it collects projection data by scanning

Number of projection images: 11

Angle of view: 40 degrees

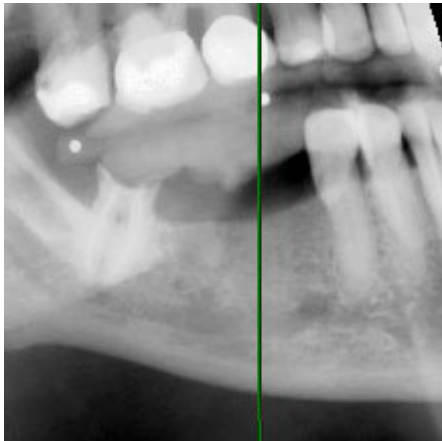
Image size: 1000×1000 pixels

The unknown vector  $f$  has 7 000 000 elements.

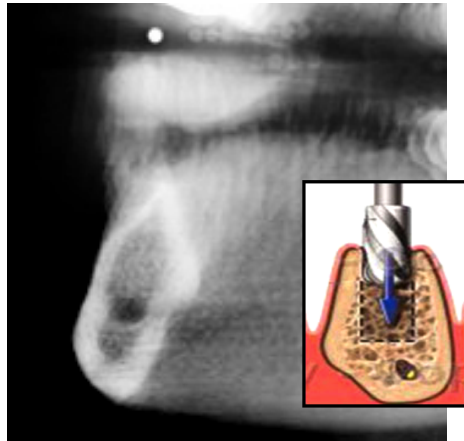




Here are example images of an actual patient:  
navigation image (left) and desired slice (right).



Kolehmainen, Vanne, S, Järvenpää, Kaipio, Lassas & Kalke 2006,  
Kolehmainen, Lassas & S 2008



Cederlund, Kalke & Welanders 2009,  
Hyvönen, Kalke, Lassas, Setälä & S  
2010, **U.S. patent 7269241**

# The radiation dose of the VT device is lowest among 3D dental imaging modalities

| Modality         | $\mu\text{Sv}$ |
|------------------|----------------|
| Head CT          | 2100           |
| CB Mercuray      | 558            |
| i-Cat            | 193            |
| NewTom 3G        | 59             |
| <b>VT device</b> | <b>13</b>      |

Ludlow, Davies-Ludlow, Brooks & Howerton 2006

