

X-ray tomography

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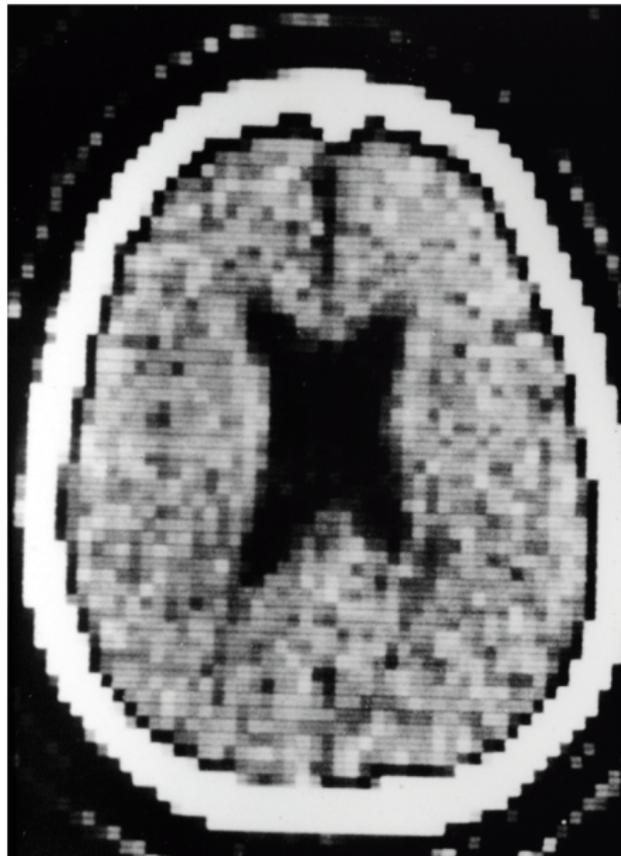
November 6, 2012



Godfrey Hounsfield and Allan McLeod Cormack were the first to develop X-ray tomography



Hounsfield (top) and Cormack received Nobel prizes in 1979.



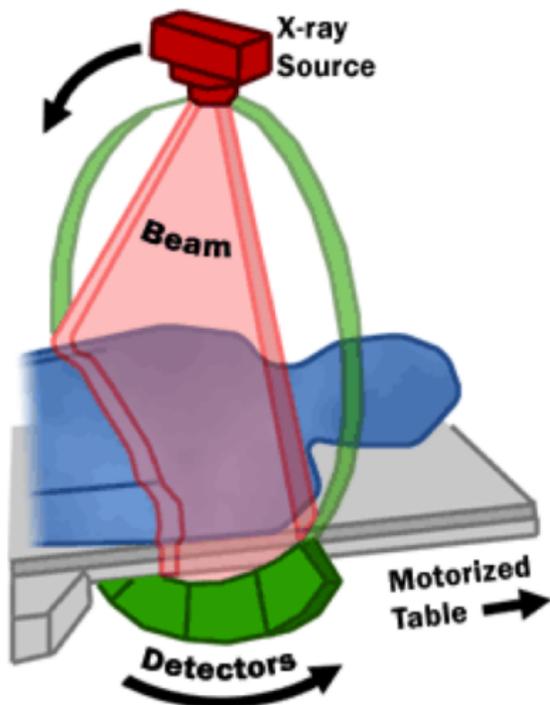
Reconstruction of a function from its line integrals was first invented by Johann Radon in 1917



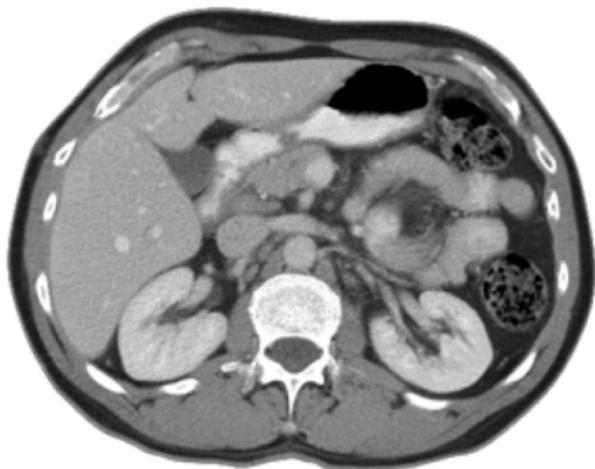
Johann Radon (1887-1956)

$$f(P) = -\frac{1}{\pi} \int_0^\infty \frac{d\overline{F}_p(q)}{q}$$

Traditional X-ray tomography requires many projection images using small angular steps



$$f(x) = \frac{1}{4\pi^2} \int_{S^1} \int_{\mathbb{R}} \frac{\frac{d}{ds}(Rf)(\theta, s)}{x \cdot \theta - s} ds d\theta$$



Due to the radiation dose, a CT scan is only appropriate for seriously ill patients

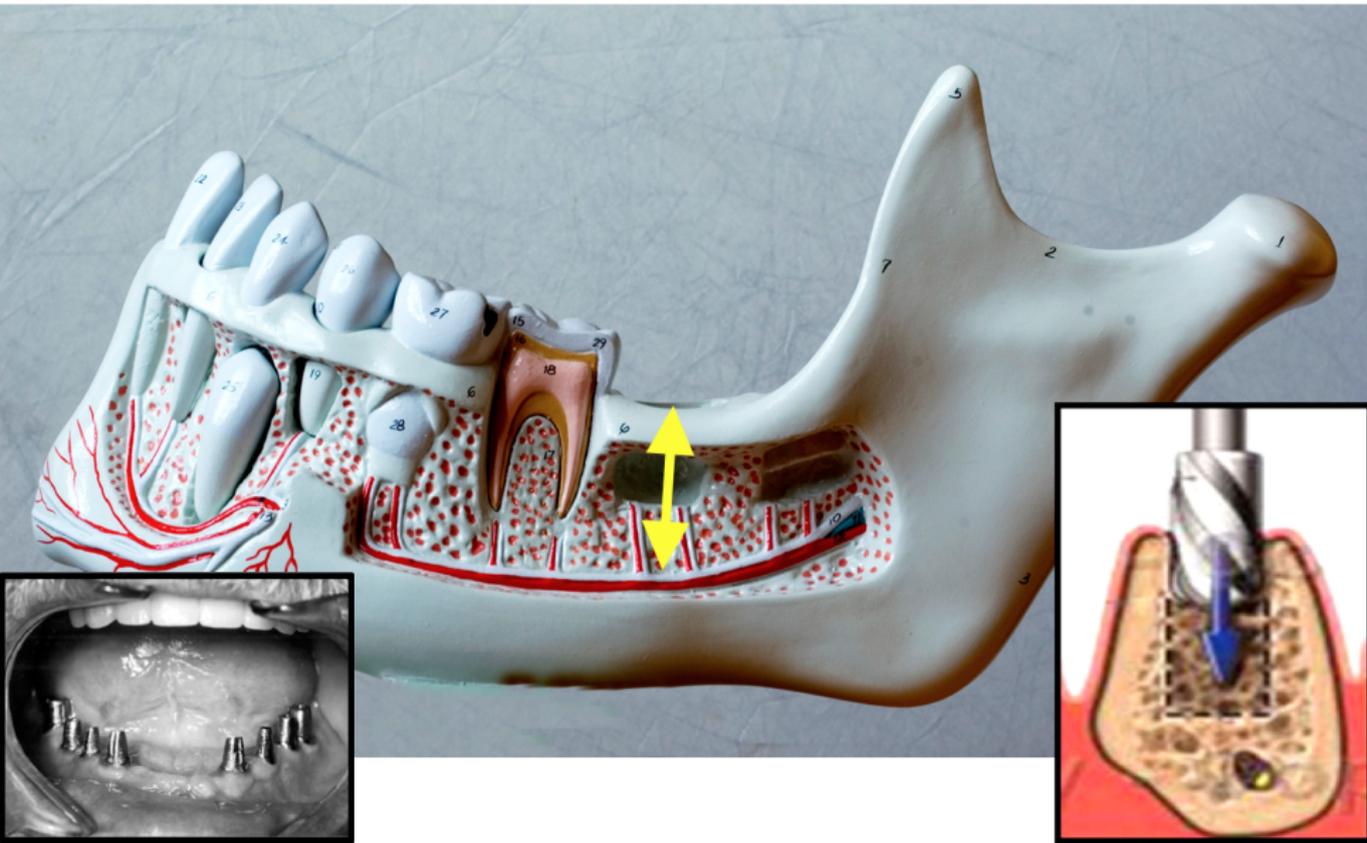
In filtered backprojection, the mathematical reconstruction formula assumes dense angular sampling of full-angle data. The inverse problem is only mildly ill-posed, but

The chosen mathematics requires high radiation dose.

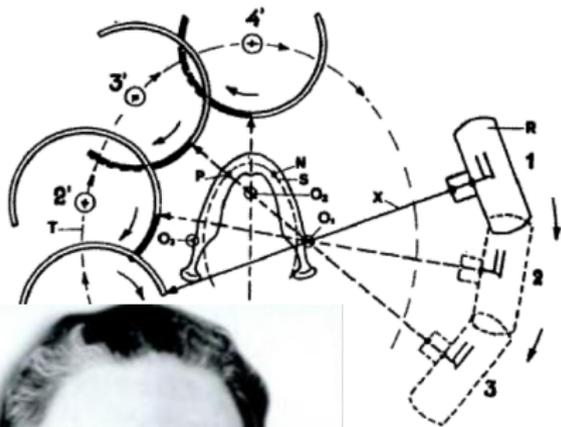
Think the opposite: take as few X-ray images as possible. The inverse problem is very ill-posed. Use advanced mathematics to form a reconstruction that is good enough for the clinical task.

The low level of radiation dose requires new mathematics and more computational power.

Application: dental implant planning, where a missing tooth is replaced with an implant



Panoramic dental imaging shows all the teeth simultaneously



Panoramic imaging was invented by Yrjö Veli Paatero in the 1950's.



Nowadays, a digital panoramic imaging device is standard equipment at dental clinics



Panoramic images are not good enough for dental implant planning because of geometric distortion.

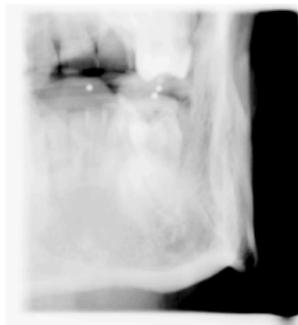
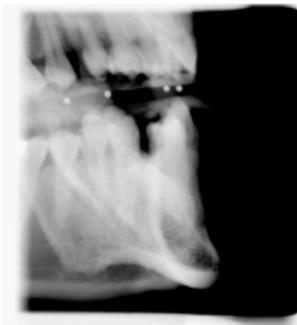
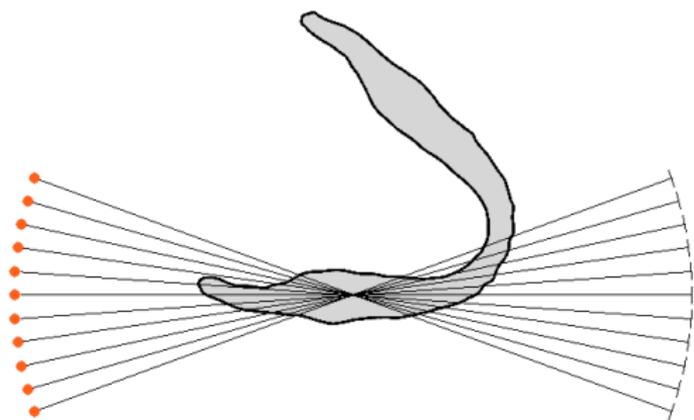


We reprogram the panoramic X-ray device so that it collects projection data by scanning

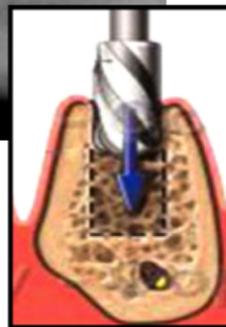
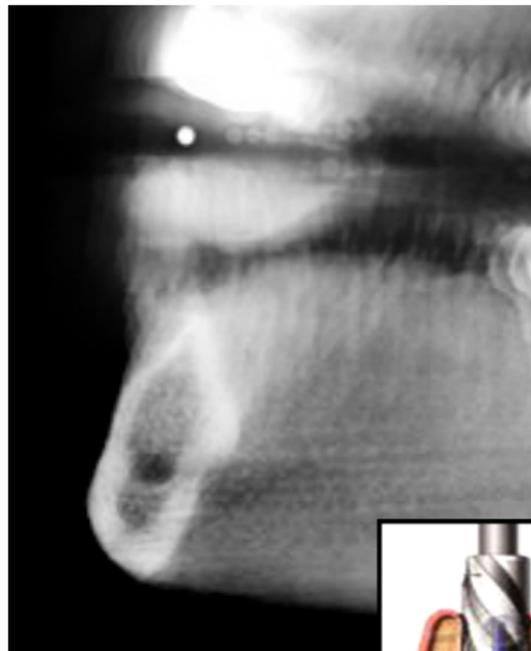
11 projection images of the mandibular area

40 degrees angle of view

1000×1000 image size, formed by a scanning movement



Here are example images of a patient



Kolehmainen, Vanne, S, Järvenpää, Kaipio, Lassas & Kalke **2006**,
Kolehmainen, Lassas & S **2008**, Cederlund, Kalke & Welander **2009**,
Hyvönen, Kalke, Lassas, Setälä & S **2010**,
United States patent 7269241

This low-dose 3D imaging technique has been commercialized by Palodex Group

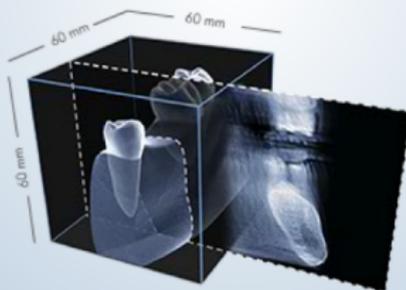
The VT device has been in the market from year 2007.

Remarkably, an existing 2D panoramic imaging device becomes a 3D imaging product just by a software update.

The core of that update is an inversion algorithm.

VT — essential information for implantology

VT option is a Narrow Beam Volumetric Tomography (NBVT) imaging tool that provides digital tomography with reliable measurements and excellent image quality for implant site evaluation.



What does VT do?

One VT image covers a cubical area of ~ 60 mm per side, producing 256 cross-sectional slices with a minimum slice thickness of 0,23 mm.

How does VT do this?

The resulting 3D model is reconstructed from a set of projection images targeted only on the region of interest. The reconstructed, wide volumetric view offers 256 slices, from which the optimal slice or any number of slices can be viewed.

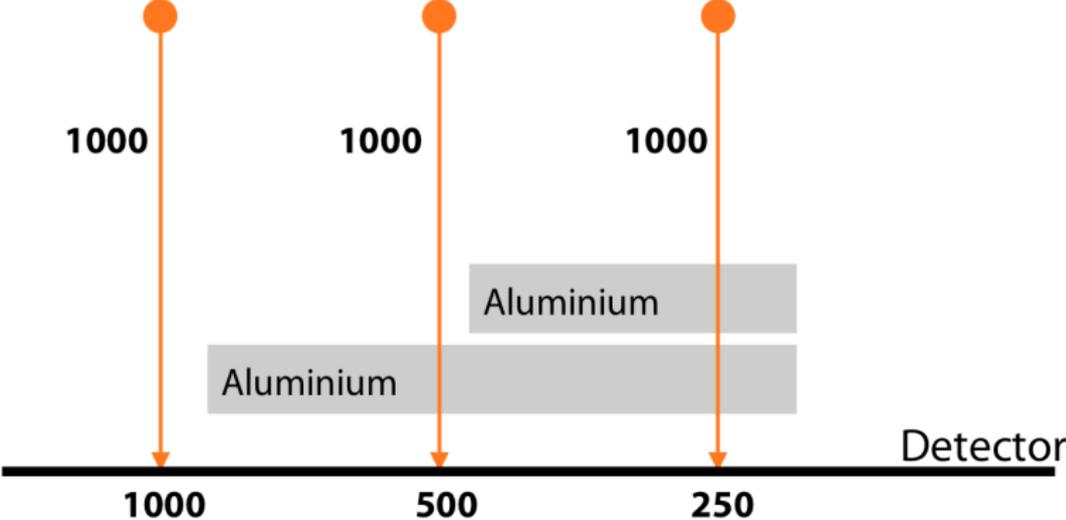
The radiation dose of the VT device is the lowest among 3D dental imaging modalities

Modality	μSv
Head CT	2100
CB Mercuray	558
i-Cat	193
NewTom 3G	59
VT device	13

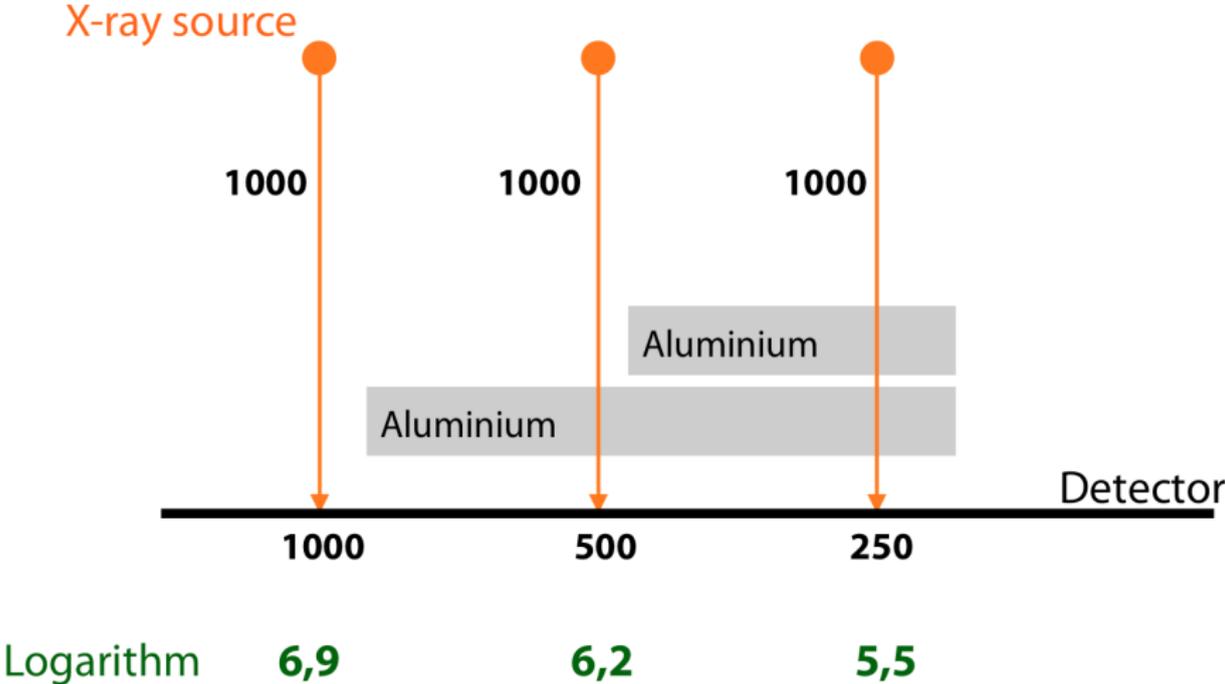
Ludlow, Davies-Ludlow, Brooks & Howerton 2006

Mathematical interpretation of X-ray measurements

X-ray source

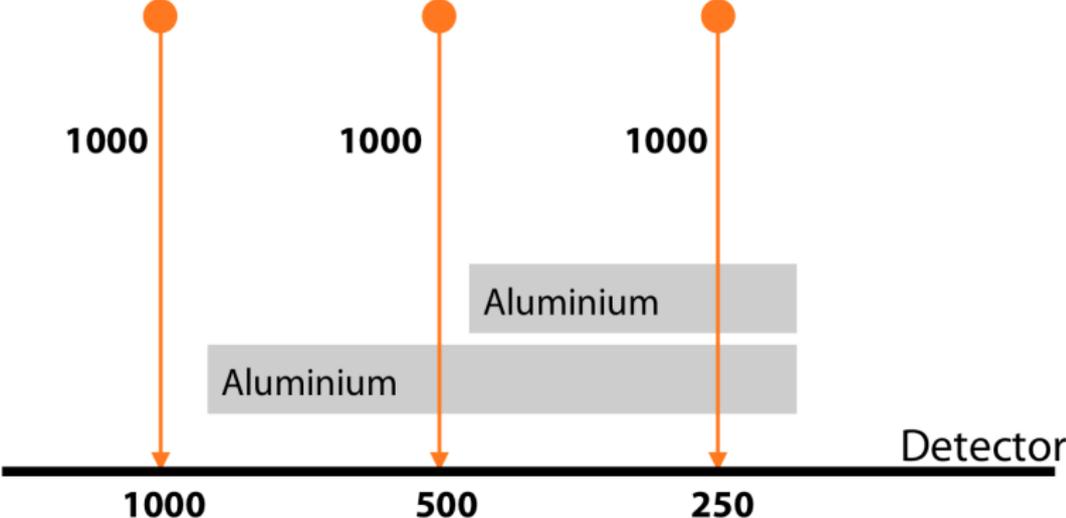


Mathematical interpretation of X-ray measurements



Mathematical interpretation of X-ray measurements

X-ray source



Logarithm

6,9

6,2

5,5

Density

0,0

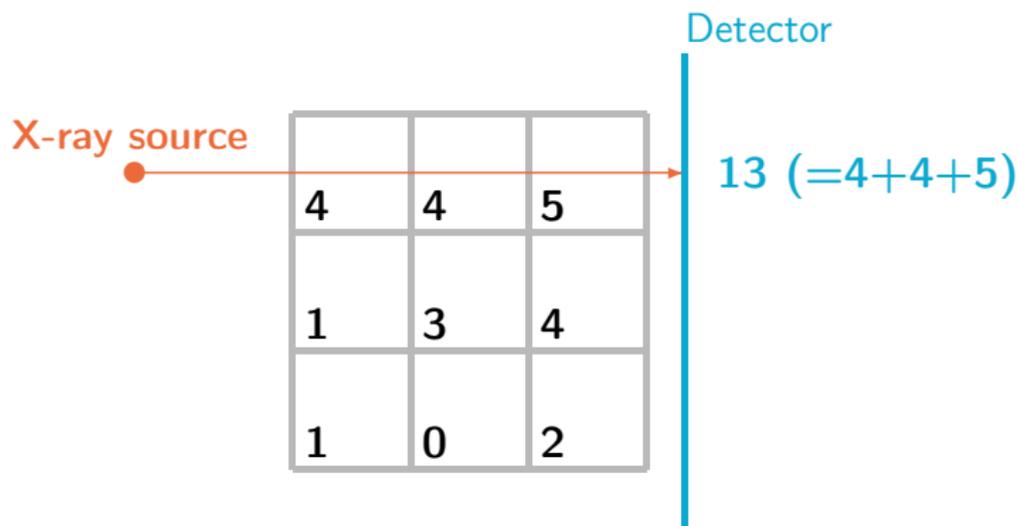
0,7

1,4

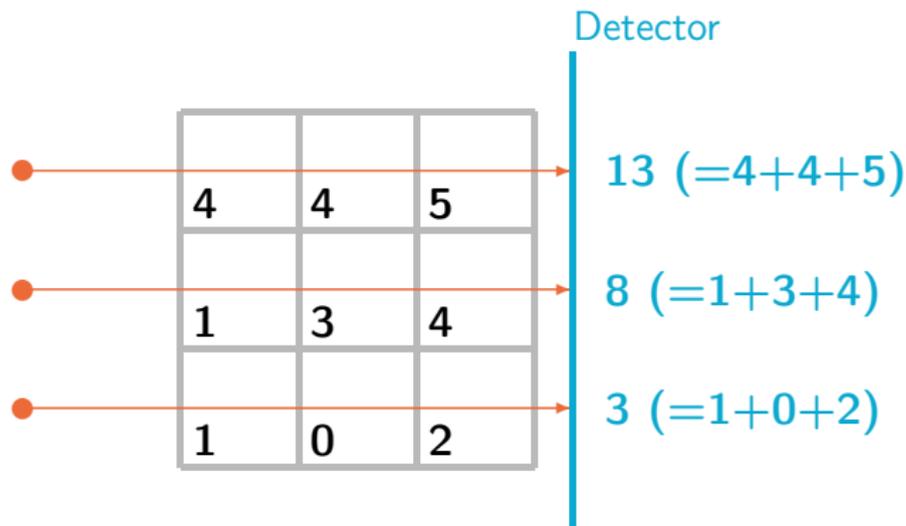
Let us study a simple two-dimensional example of tomographic imaging

4	4	5
1	3	4
1	0	2

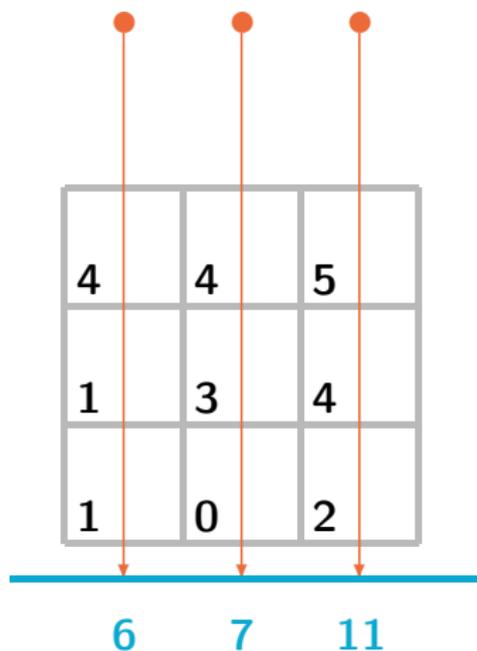
Tomography is based on measuring densities of matter using X-ray attenuation data



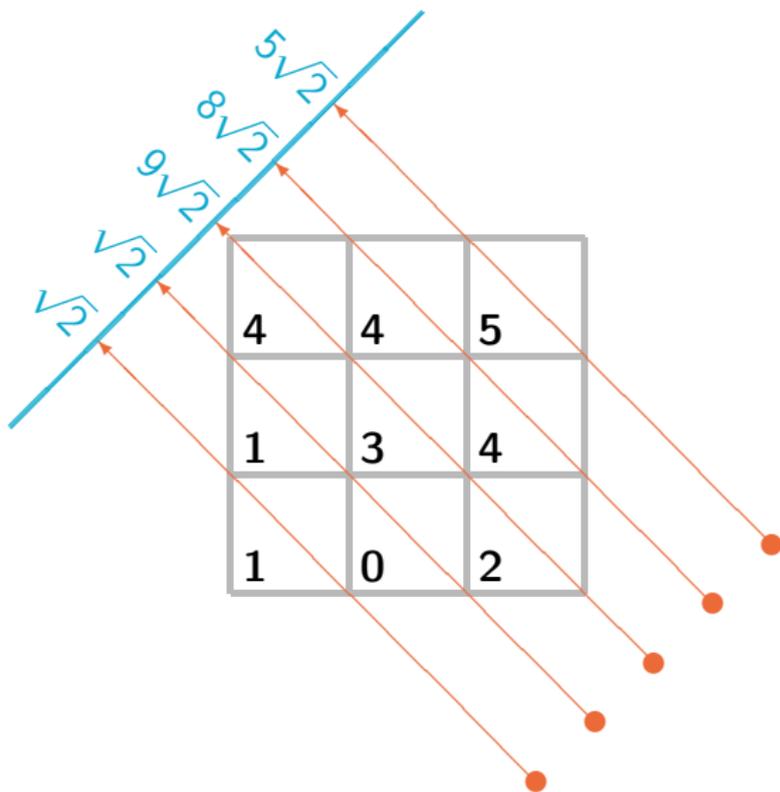
A projection image is produced by parallel X-rays and several detector pixels (here three pixels)



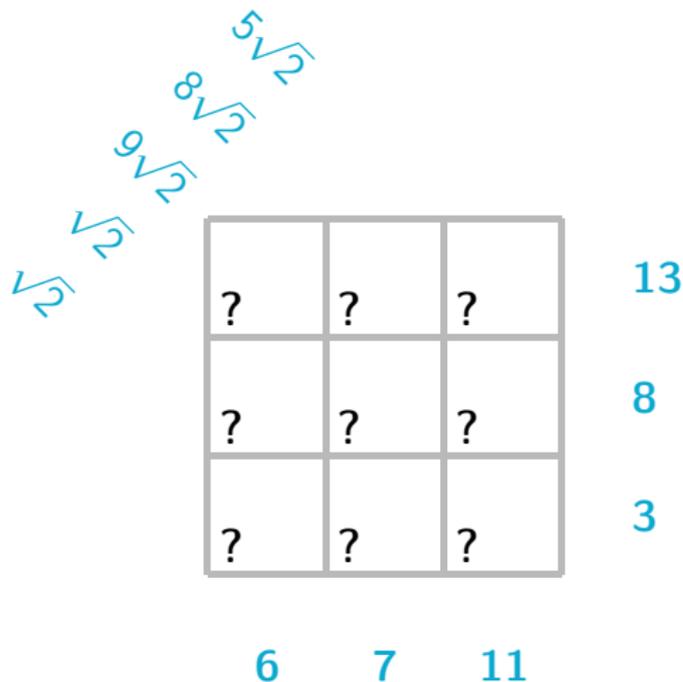
For tomographic imaging it is essential to record projection images from different directions



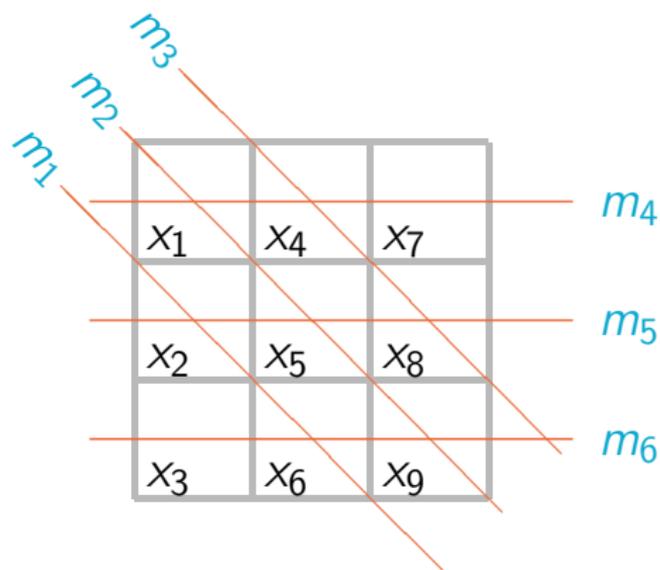
The length of X-rays traveling inside each pixel is important, thus here the square roots



The inverse problem of tomography is to reconstruct the interior from X-ray data



We write the reconstruction problem in matrix form and assume Gaussian noise



$$x = \begin{bmatrix} x_1 \\ x_2 \\ x_3 \\ x_4 \\ x_5 \\ x_6 \\ x_7 \\ x_8 \\ x_9 \end{bmatrix}, \quad m = \begin{bmatrix} m_1 \\ m_2 \\ m_3 \\ m_4 \\ m_5 \\ m_6 \end{bmatrix},$$

$$m = Ax$$

Our measurement model is $m = Ax + \varepsilon$ with independently distributed Gaussian noise (white noise) with standard deviation $\sigma > 0$.

This is the matrix equation $Ax = m$ related to the measurement on the previous slide

$$\begin{bmatrix} 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 \\ \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} \\ 0 & 0 & 0 & \sqrt{2} & 0 & 0 & 0 & \sqrt{2} & 0 \\ 1 & 0 & 0 & 1 & 0 & 0 & 1 & 0 & 0 \\ 0 & 1 & 0 & 0 & 1 & 0 & 0 & 1 & 0 \\ 0 & 0 & 1 & 0 & 0 & 1 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} x_1 \\ x_2 \\ x_3 \\ x_4 \\ x_5 \\ x_6 \\ x_7 \\ x_8 \\ x_9 \end{bmatrix} = \begin{bmatrix} m_1 \\ m_2 \\ m_3 \\ m_4 \\ m_5 \\ m_6 \end{bmatrix}.$$

