

# Structure of tomographic X-ray data

A scenic view of a rocky coastline. The foreground shows a sandy beach with gentle waves washing onto it. In the middle ground, a large, white-capped wave is breaking, creating a spray of water. The background features rugged, golden-brown rock formations and cliffs extending into the distance under a clear blue sky. The overall scene is bright and clear, suggesting a sunny day.

**Samuli Siltanen**

**Department of Mathematics and Statistics**

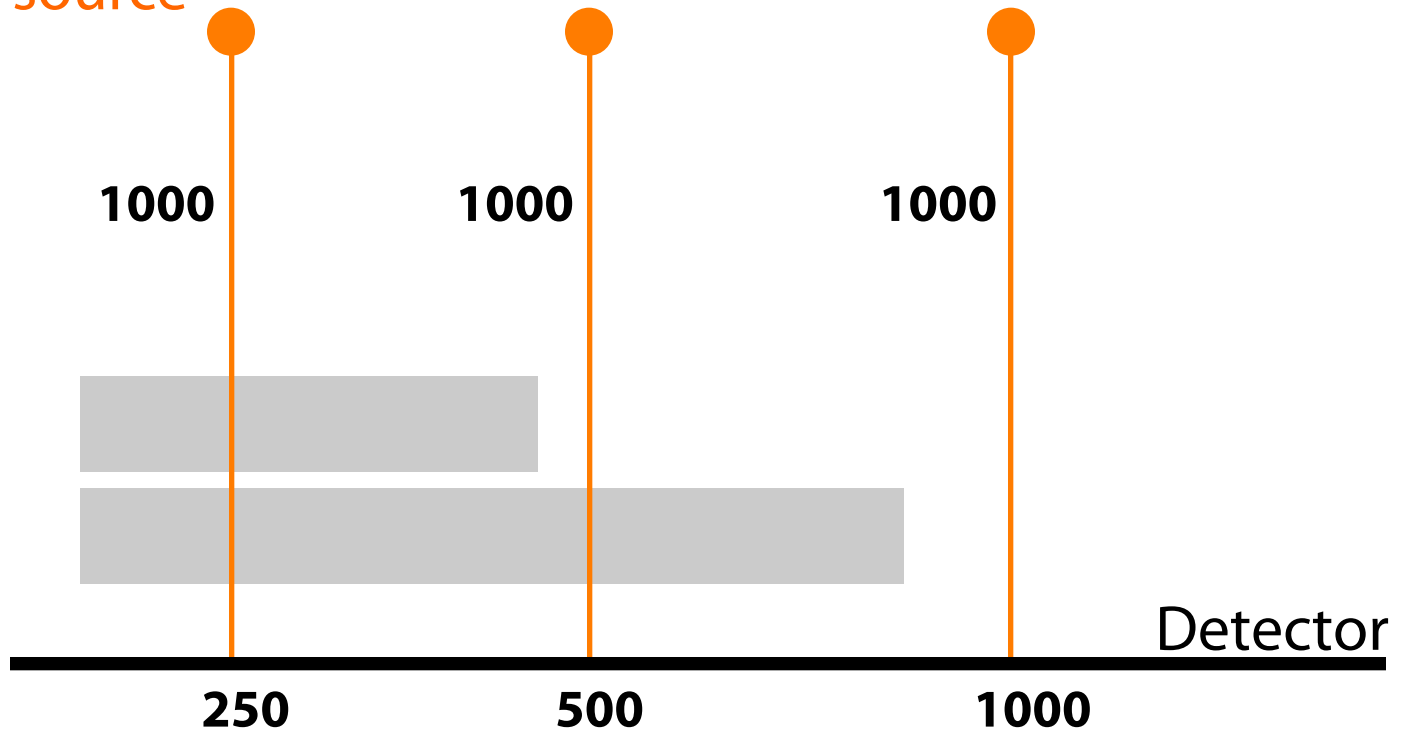
**University of Helsinki**

Course on computational inverse problems



# X-ray images as measurements

X-ray source



Logarithm

**5,5**

**6,2**

**6,9**

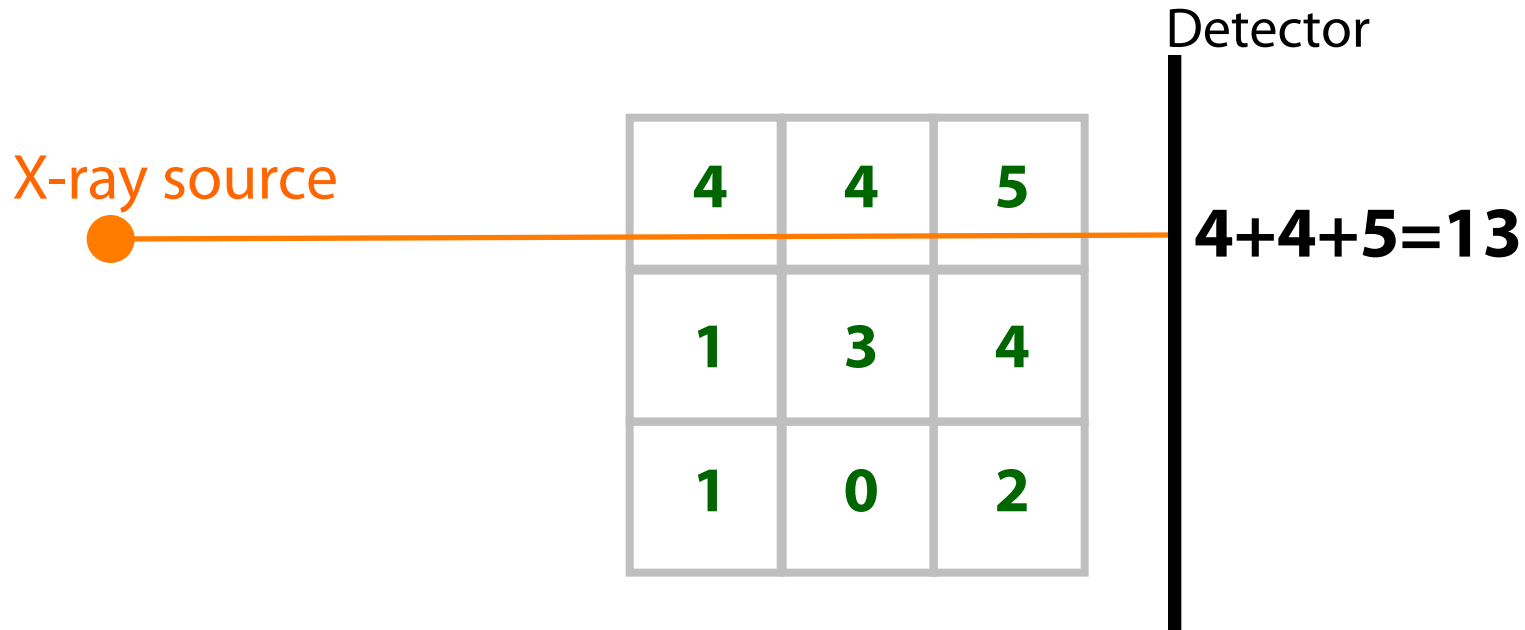
Density

**1,4**

**0,7**

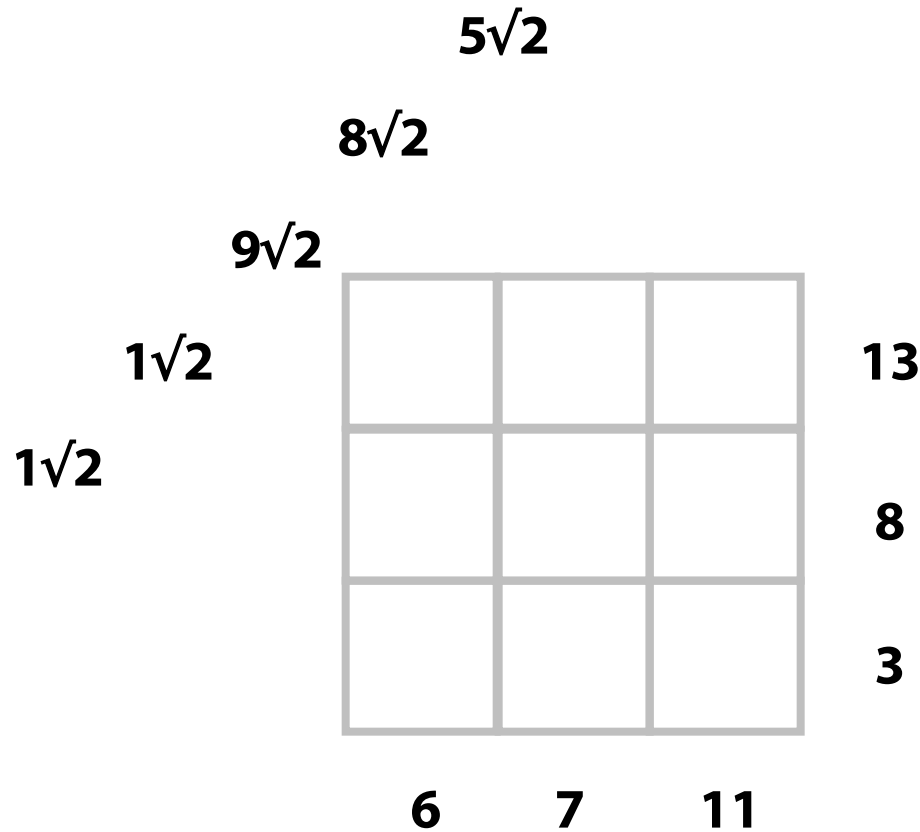
**0,0**

# Every X-ray measures the sum of attenuation through tissue



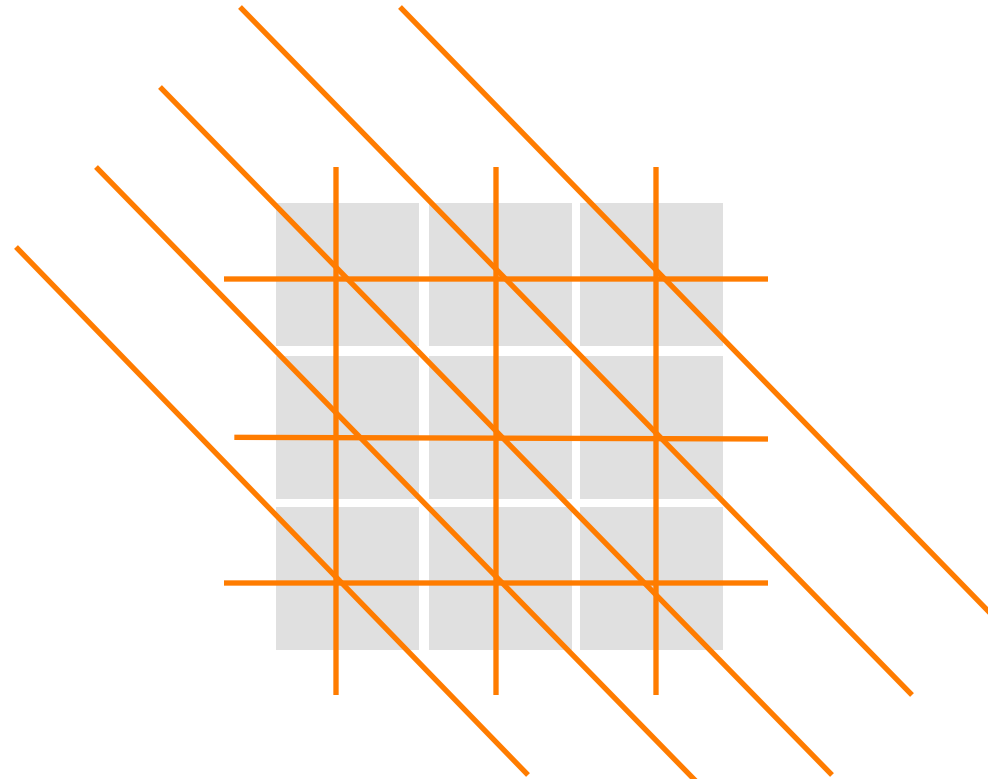


# Inverse problem of tomography is to find the tissue from radiographs

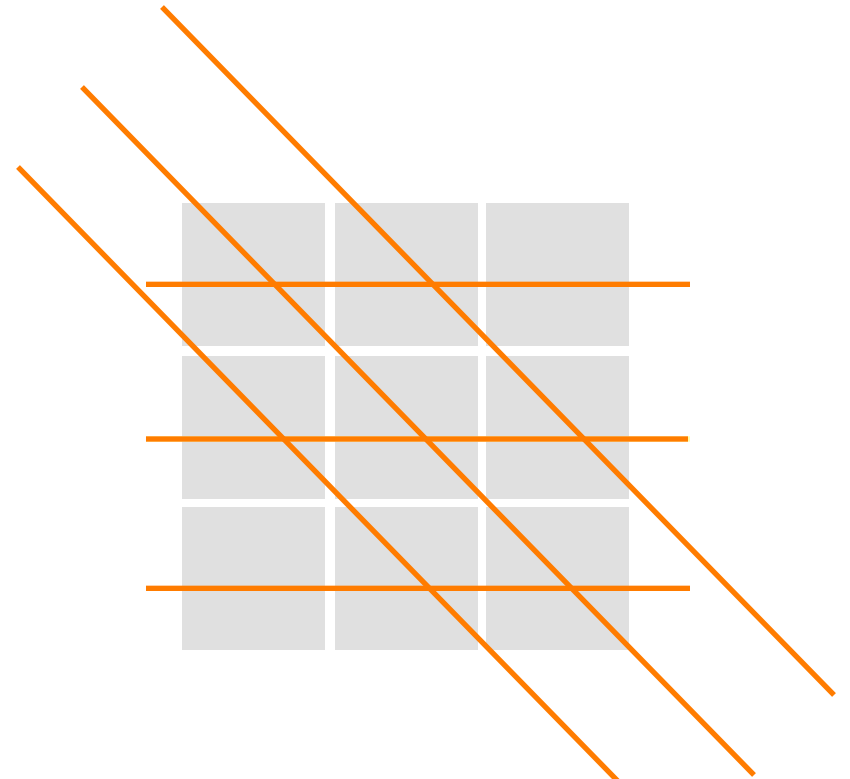


9 unknowns, 11 linear equations

# The limited angle problem is harder than the full angle problem



9 unknowns,  
11 linear equations



9 unknowns,  
6 linear equations





# We write the reconstruction problem in matrix form and assume Gaussian noise

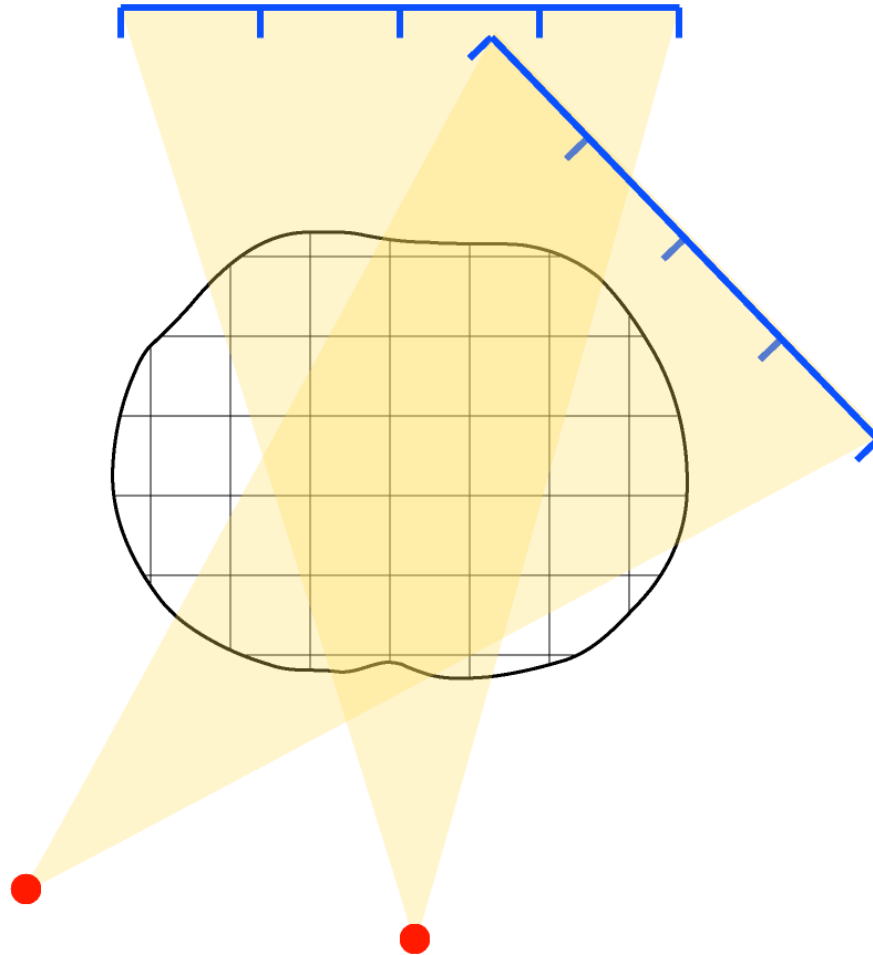
			m3		
	m2				
m1		x1	x4	x7	m4
		x2	x5	x8	m5
		x3	x6	x9	m6

$$x = [x_1, x_2, \dots, x_9]^T$$
$$m = [m_1, m_2, \dots, m_6]^T$$

$$Ax = m$$

We consider the measurement model  $m = Ax + \varepsilon$  with additive Gaussian noise  $\varepsilon$  of standard deviation  $\sigma$ .

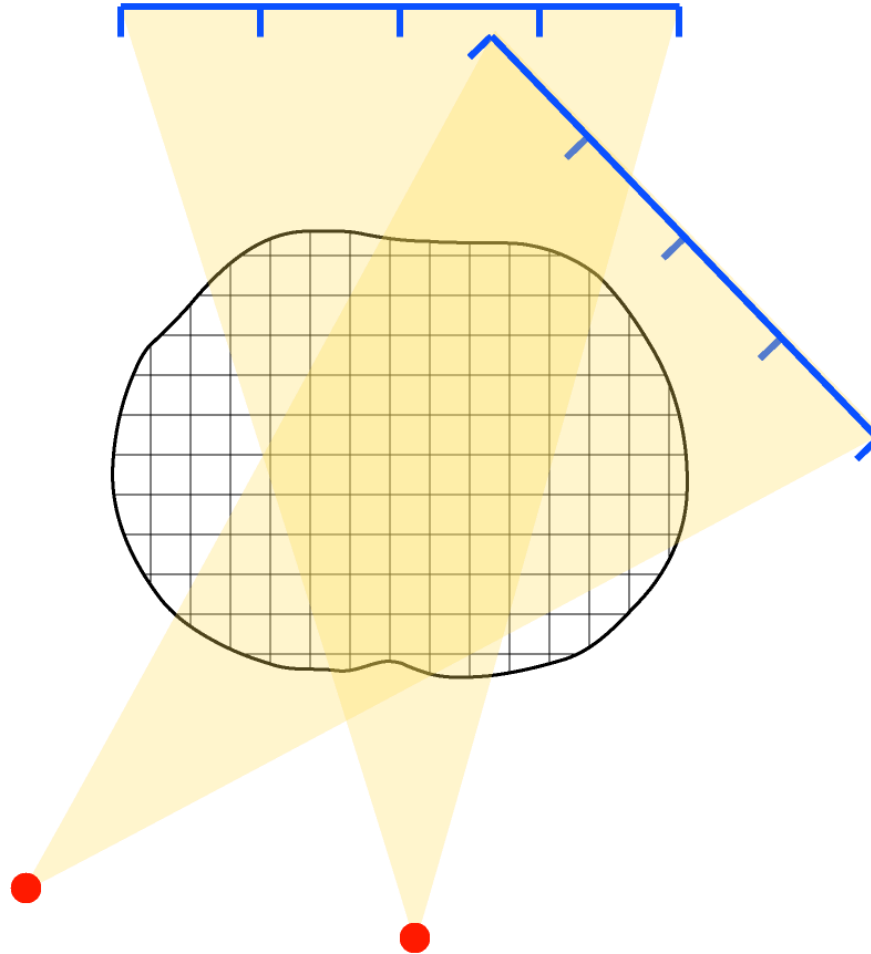
**Number of data is k, number of unknowns is n**



$$k=8$$

$$n=48$$

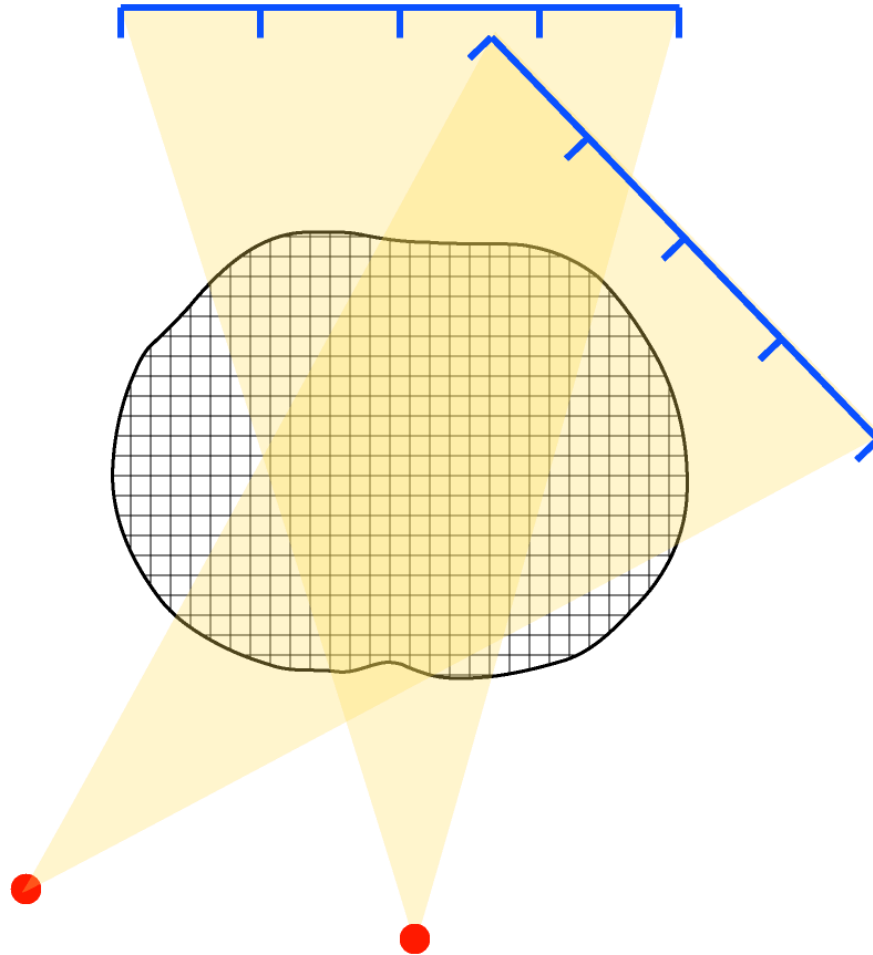
**Number of data is  $k$ , number of unknowns is  $n$**



$$k=8$$

$$n=156$$

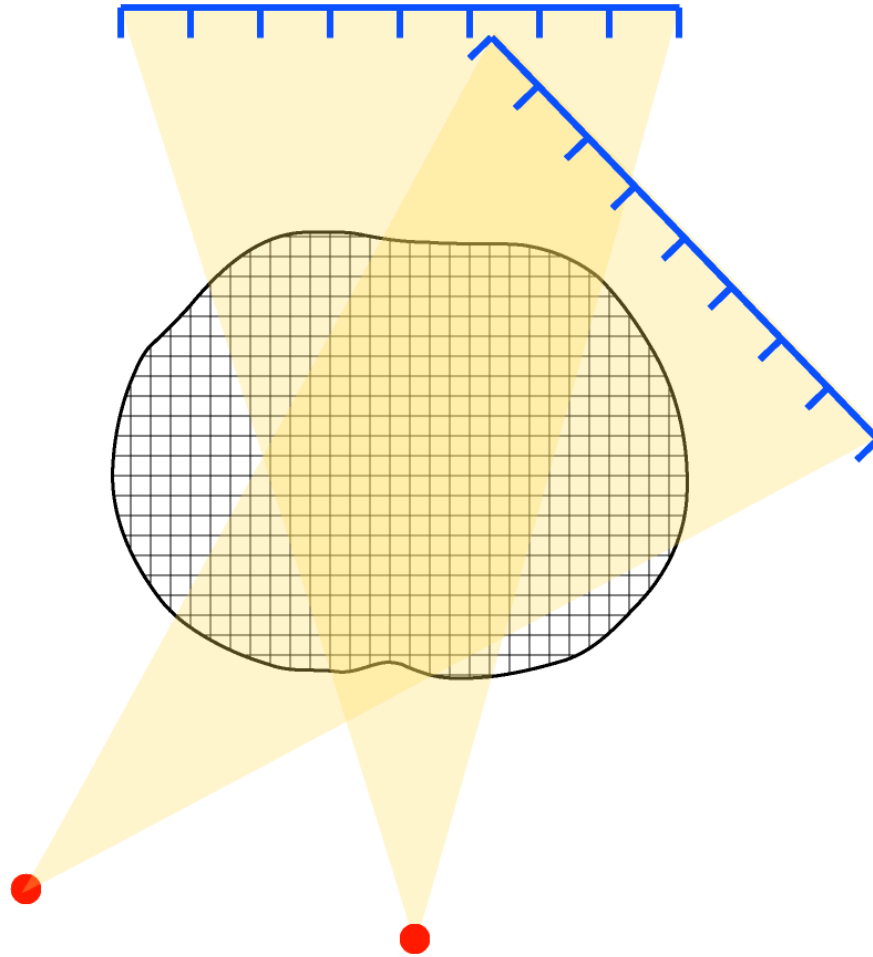
**Number of data is  $k$ , number of unknowns is  $n$**



$$k=8$$

$$n=440$$

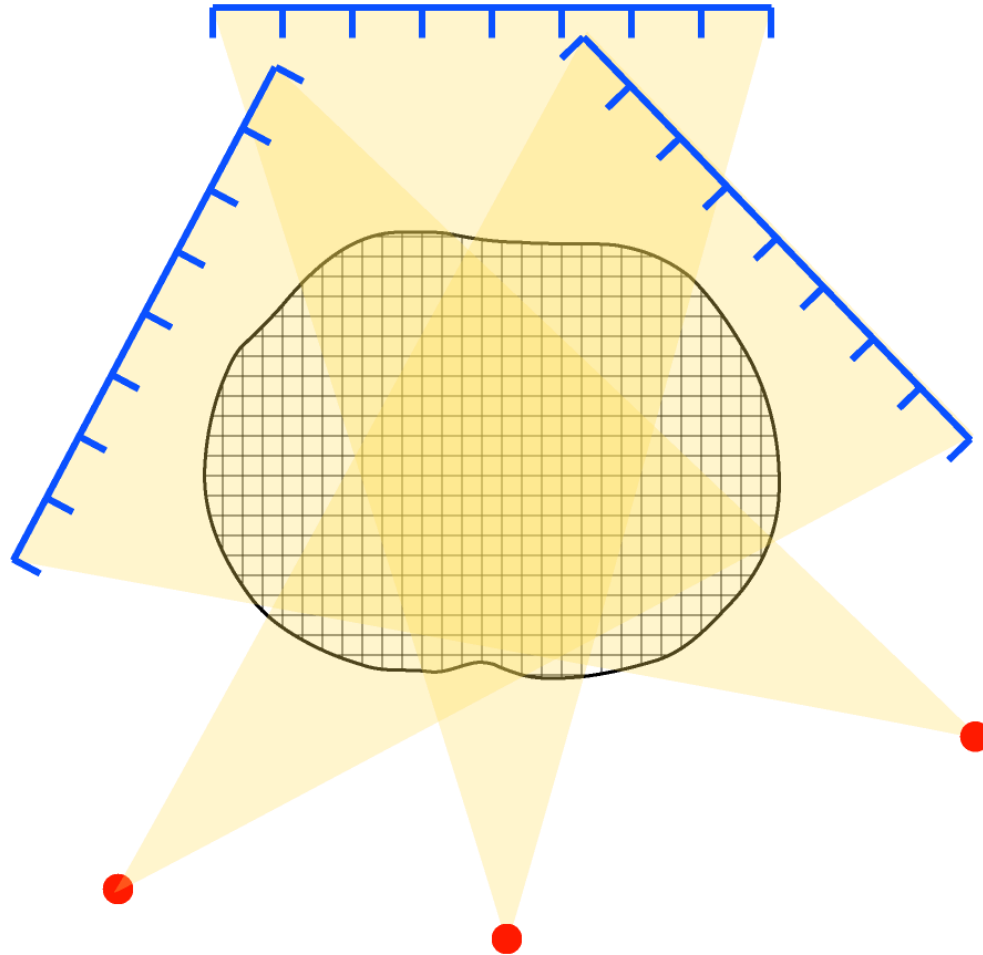
**Number of data is  $k$ , number of unknowns is  $n$**



$$k=16$$

$$n=440$$

**Number of data is  $k$ , number of unknowns is  $n$**

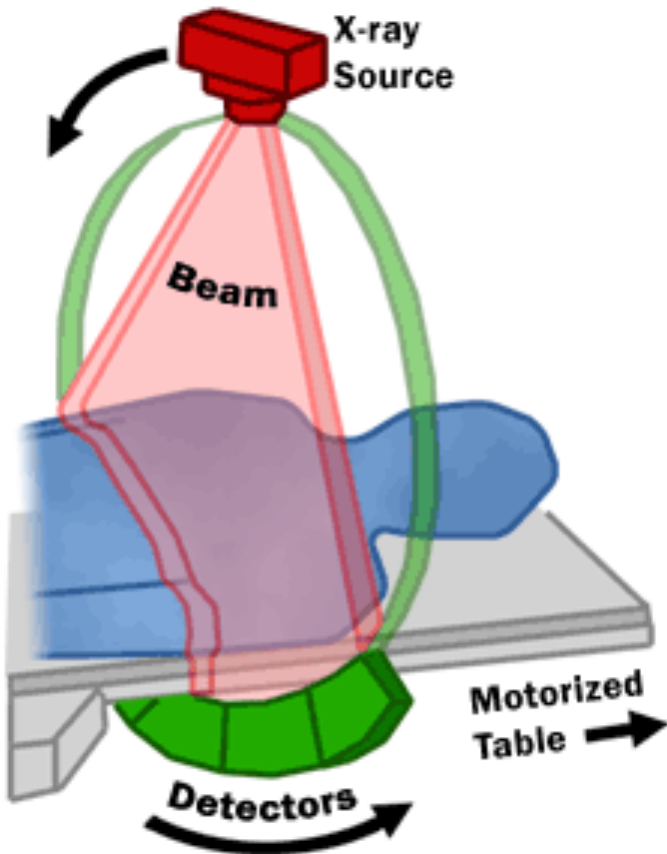


$$k=24$$

$$n=440$$

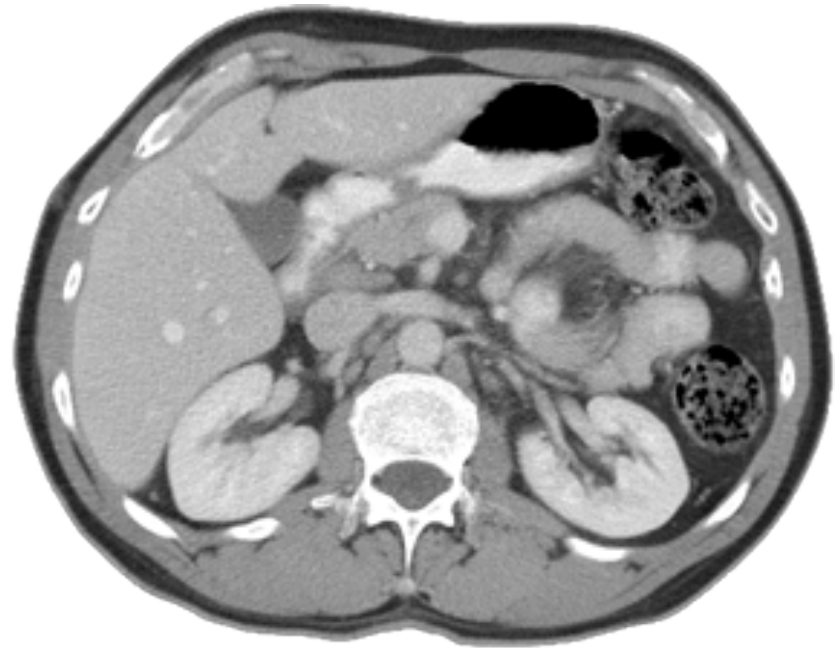
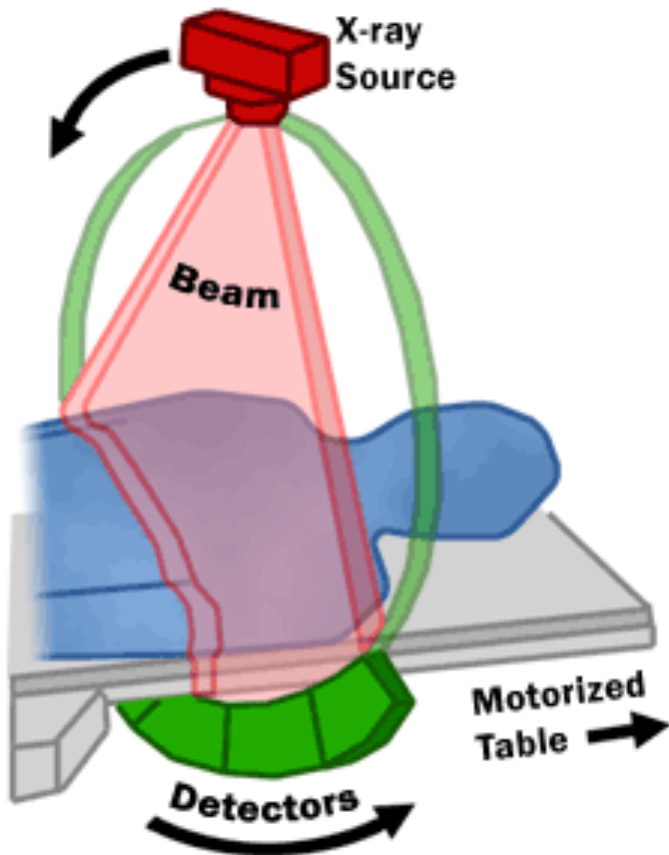
# To explain low-dose 3D imaging, let's start by discussing traditional 3D imaging

X-ray attenuation data is collected from 180 directions separately for each two-dimensional slice.



# Using a reconstruction algorithm, inner structure in the slice is revealed

This is called computerized tomography (CT).

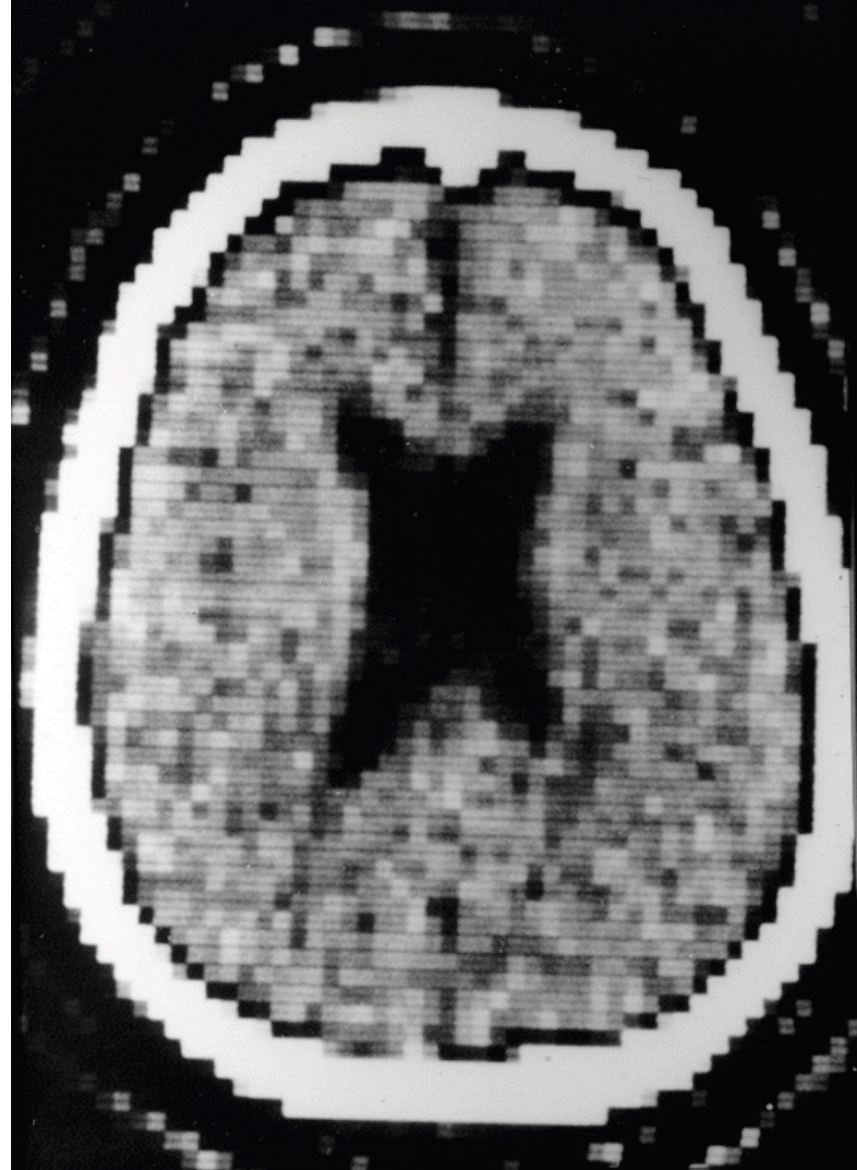




# Godfrey Hounsfield and Allan McLeod Cormack were the first to develop X-ray tomography



Nobel prize was awarded to Hounsfield (top) and Cormack in 1979.



# Reconstruction of a function from its line integrals was first invented by



**Johann Radon** (1887-1956).

This is the famous inversion formula from 1917 for the Radon transform  $Rf$  of a function  $f$ :

$$f(x) = \frac{1}{4\pi^2} \int_{S^1} \int_{\mathcal{R}} \frac{\frac{d}{ds}(Rf)(\theta, s)}{x \cdot \theta - s} ds d\theta$$



## Filtered back-projection

$$f(x) = \frac{1}{4\pi^2} \int_{S^1} \int_{\mathcal{R}} \frac{\frac{d}{ds}(Rf)(\theta, s)}{x \cdot \theta - s} ds d\theta$$



Filtered back-projection (FBP) is mathematical technology used on a daily basis in hospitals around the world. The quality of 3D reconstruction using FBP is excellent.

**However, a comprehensive data set is mandatory for FBP.**



# Due to the radiation dose, a CT scan is only appropriate for seriously ill patients

In filtered backprojection, the mathematical reconstruction formula assumes dense angular sampling of full-angle data: **the chosen mathematics requires high radiation dose.**

Think the opposite: take as few X-ray images as possible and use tailor-made mathematics to form a reconstruction that is good enough for the clinical task at hand. Then **the low level of radiation dose requires new mathematics and more computational power.**

# A series of projects started in 2001 aiming for a new type of low-dose 3D imaging

The goal was a mathematical algorithm with

**Input:** small number of digital X-ray images  
taken with any X-ray device

**Output:** three-dimensional reconstruction  
with high enough quality for the clinical task at hand

Products of Instrumentarium Imaging in 2001:



# This work was done in 2001-2010 jointly with

Nuutti Hyvönen  
Seppo Järvenpää  
Jari Kaipio  
Martti Kalke  
Petri Koistinen  
Ville Kolehmainen  
Matti Lassas  
Jan Moberg  
Kati Niinimäki  
Juha Pirttilä  
Maaria Rantala  
Eero Saksman  
Henri Setälä  
Erkki Somersalo  
Antti Vanne  
Simopekka Vänskä  
Richard L Webber



GE Healthcare

The logo for Palodex Group, featuring the text 'PALODEX GROUP' in a white, uppercase, sans-serif font on a dark blue rectangular background with a small yellow square in the top right corner.

PALODEX GROUP

# Essential history of the three projects:

**Academic members:** Inverse problems research groups in  
University of Helsinki,  
University of Eastern Finland,  
Aalto University and  
Tampere University of Technology  
(all located in Finland)

## **Industrial members:**

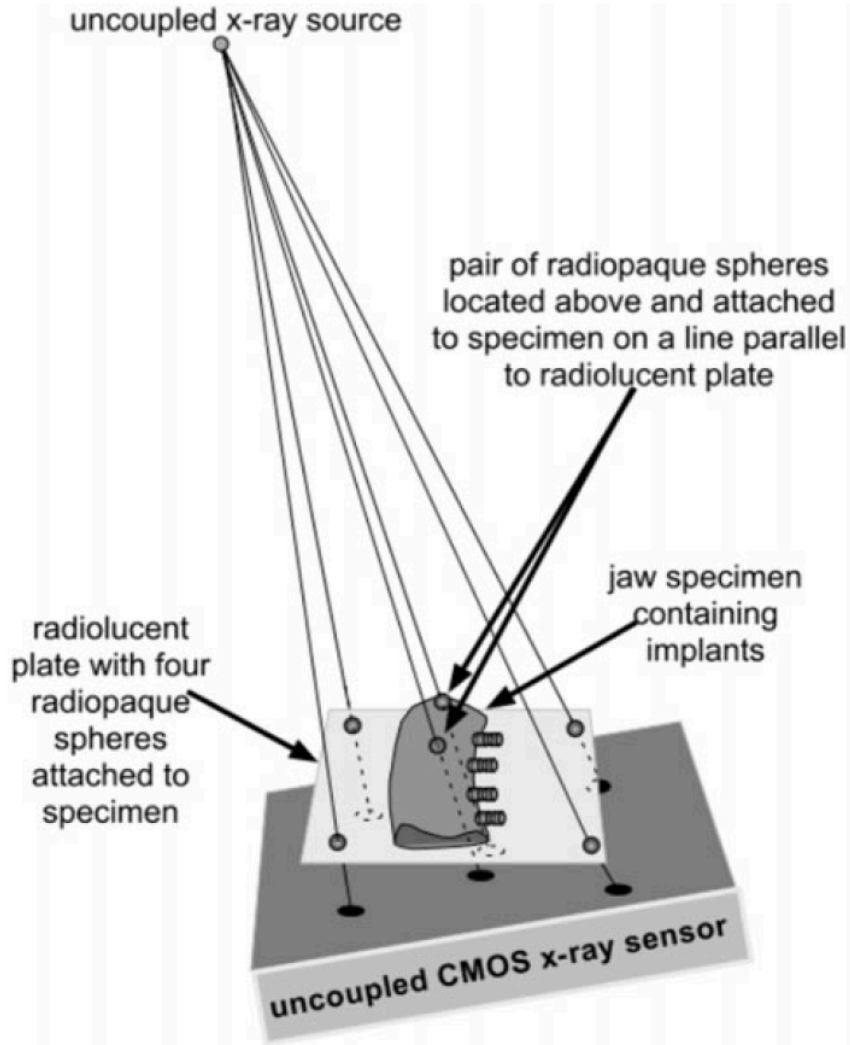
**2001-2002** Instrumentarium Imaging

**2003-2004** GE Healthcare

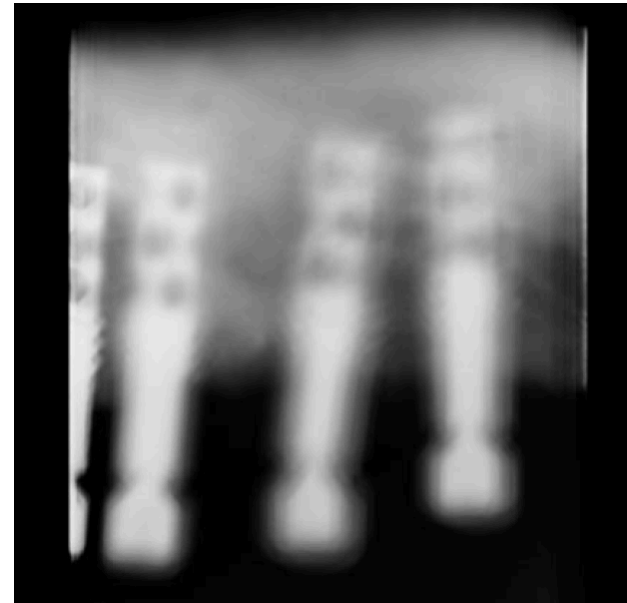
**2005-2007** PaloDEX Group

**Funding** by Finnish Technology Agency (TEKES).

# Tuned Aperture Computed Tomography (TACT) was the starting point of our research



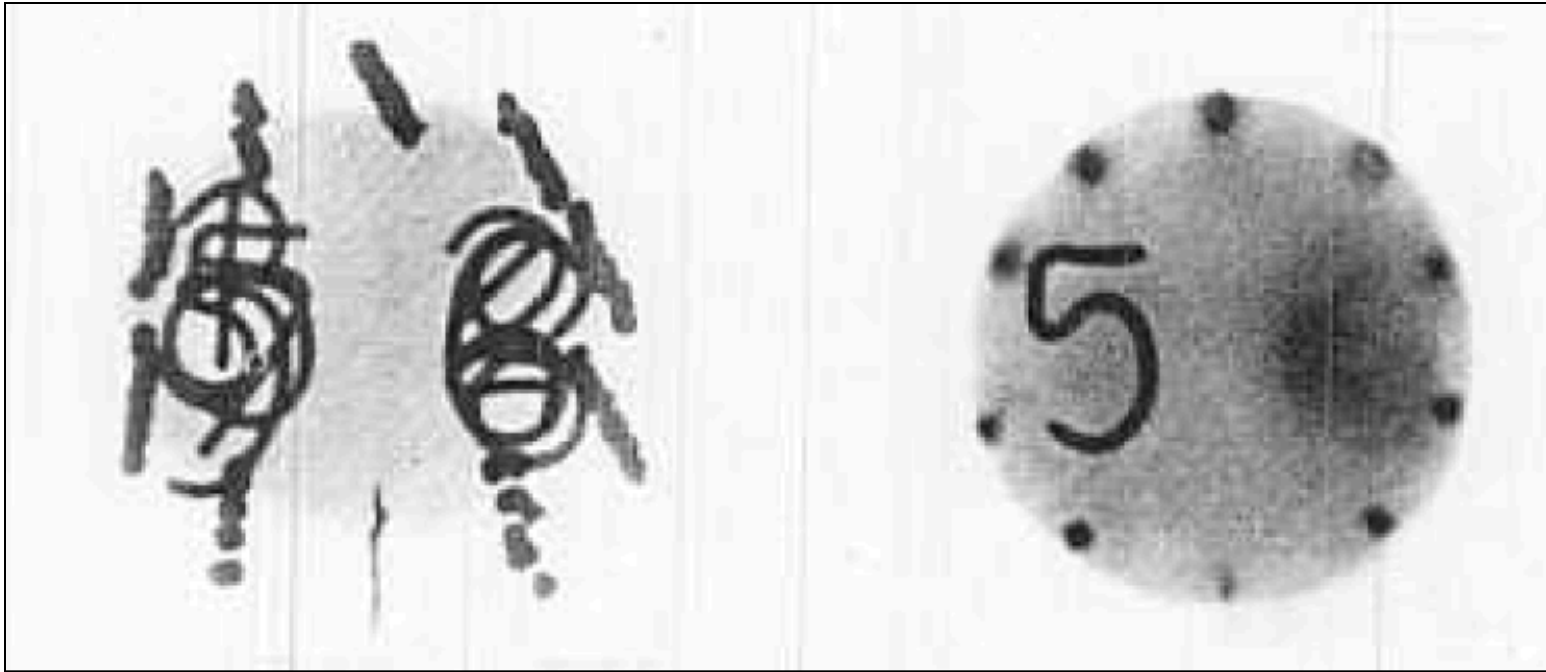
Instrumentarium Corp.  
licensed Richard Webber's  
tomosynthesis-based  
TACT patent in 1999.



Linnenbrugger, Webber and Lehmann 2002,  
US Patent 6289235 (Webber & Horton 1998)



# Tomosynthesis can be dated back to the work of Ziedses des Plantes in 1932



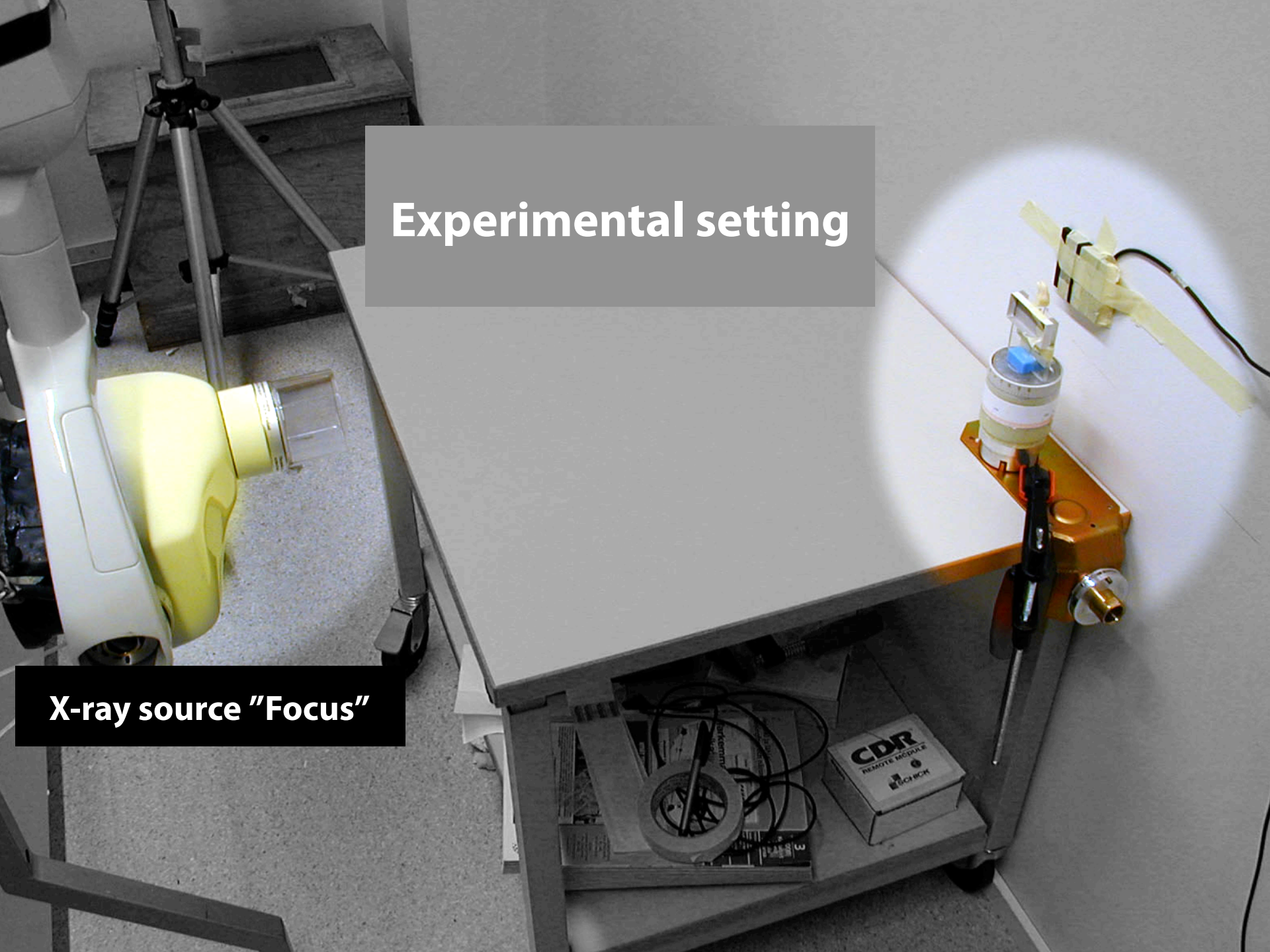
EINE NEUE METHODE ZUR DIFFERENZIERUNG IN  
DER RÖNTGENOGRAPHIE (PLANIGRAPHIE)<sup>1</sup>

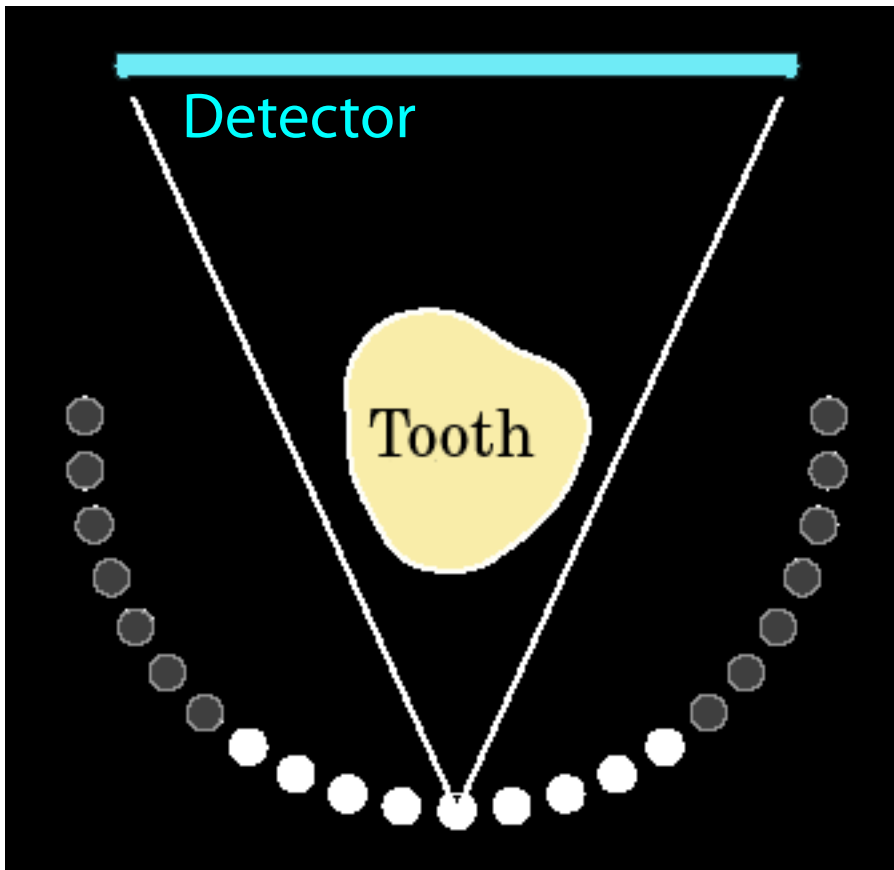
von

*B. G. Ziedses des Plantes*

# Experimental setting

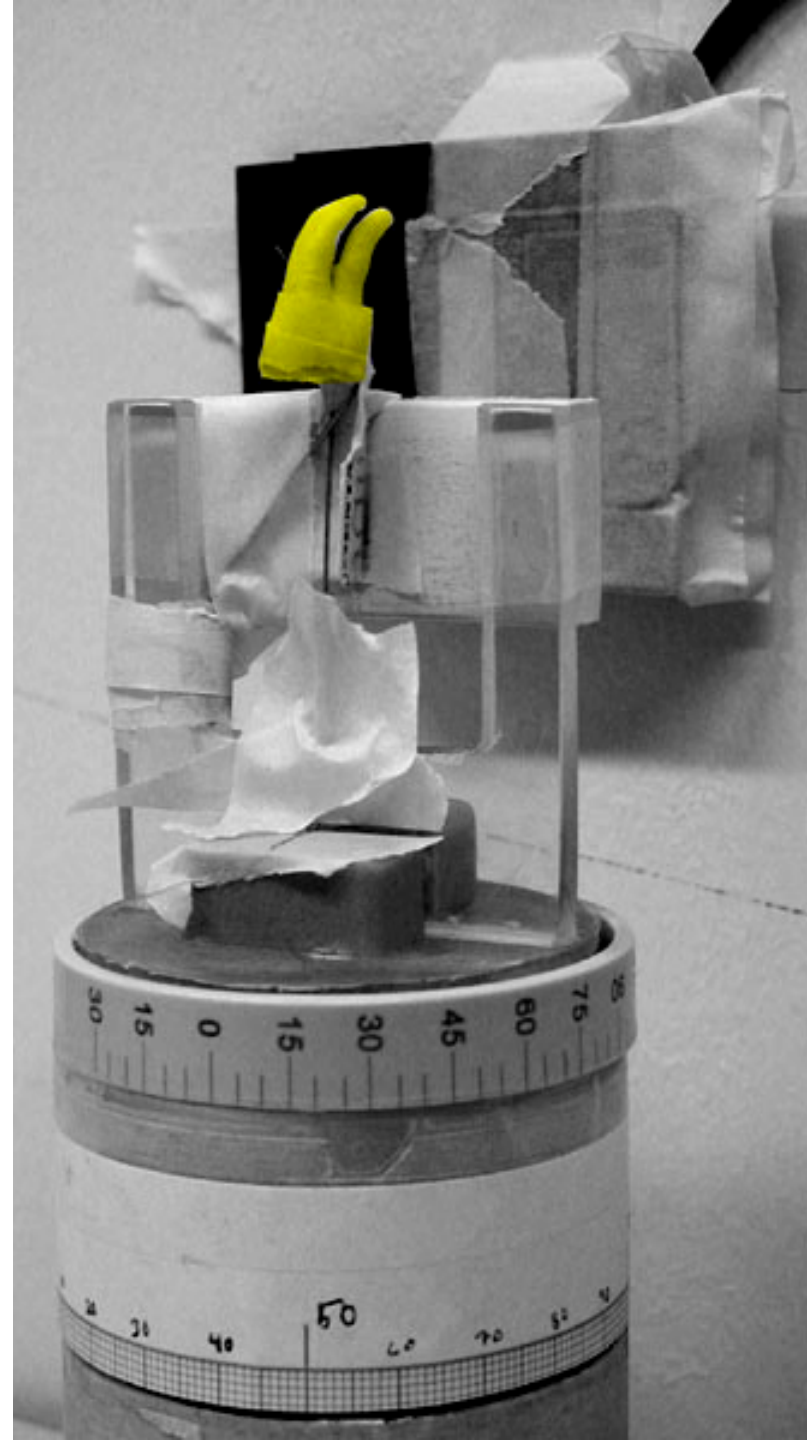
X-ray source "Focus"



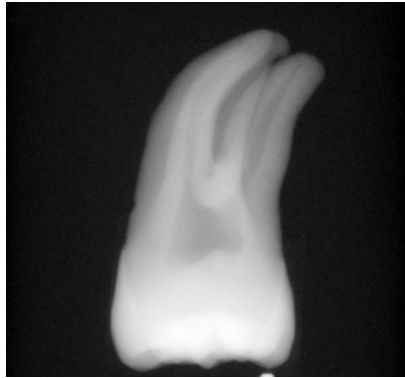


X-ray source positions  
Full data: 23 angles, 187 degrees  
Limited data: 9 angles, 68 degrees  
Almost parallel beam geometry!

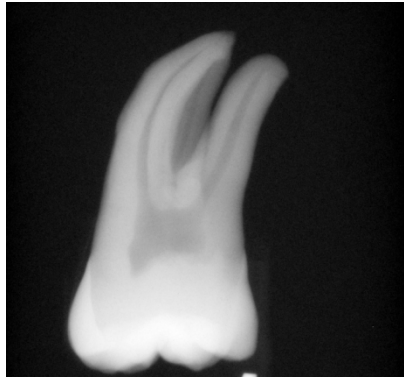
Tooth donated to science  
by Helena Sarlin. Thanks!



# The projection images look like this



0



30

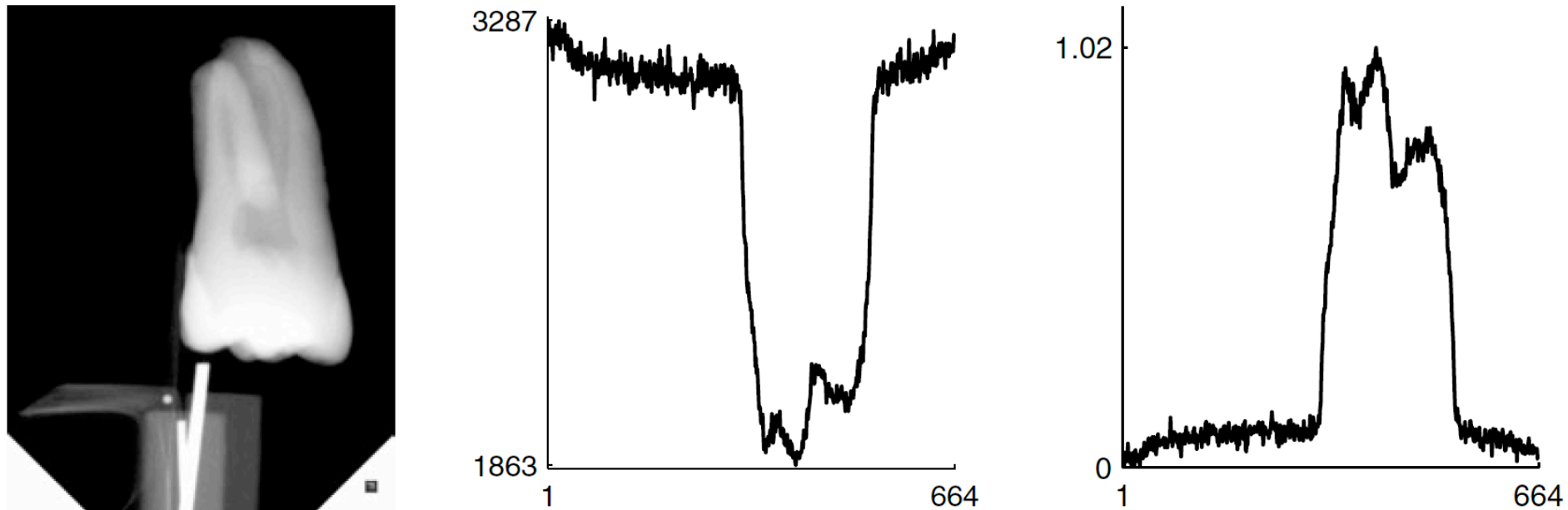


60



90

# We stack 400 two-dimensional tomographic problems using the projection data line by line



**Figure 2.** Left:  $872 \times 664$  projection radiograph from the tooth phantom. Note that the image is shown with inverted colourmap (i.e., black corresponds to high photon counts). Middle: pixel values of the 200th row from the raw projection radiograph. Right: same row in the form of tomographic attenuation data.

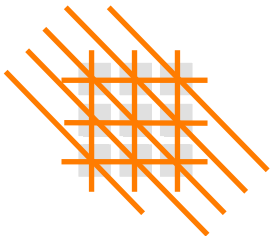
# These are the dimensions of each of the 400 two-dimensional tomographic problems

Computational domain is a square with 26mm long sides.

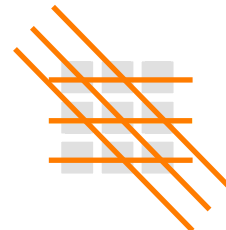
We divide the square into  $166 \times 166 = \mathbf{27556}$  pixels.

Full angle data is collected from 23 directions, each having 664 data points. Thus the number of measurements is **15272**.

Limited angle data is collected from 9 directions, each having 664 data points. Thus the number of measurements is **5976**.



Compare:  
**11** measurements,  
**9** pixels



Compare:  
**6** measurements,  
**9** pixels

# Horizontal slices:

**truth**

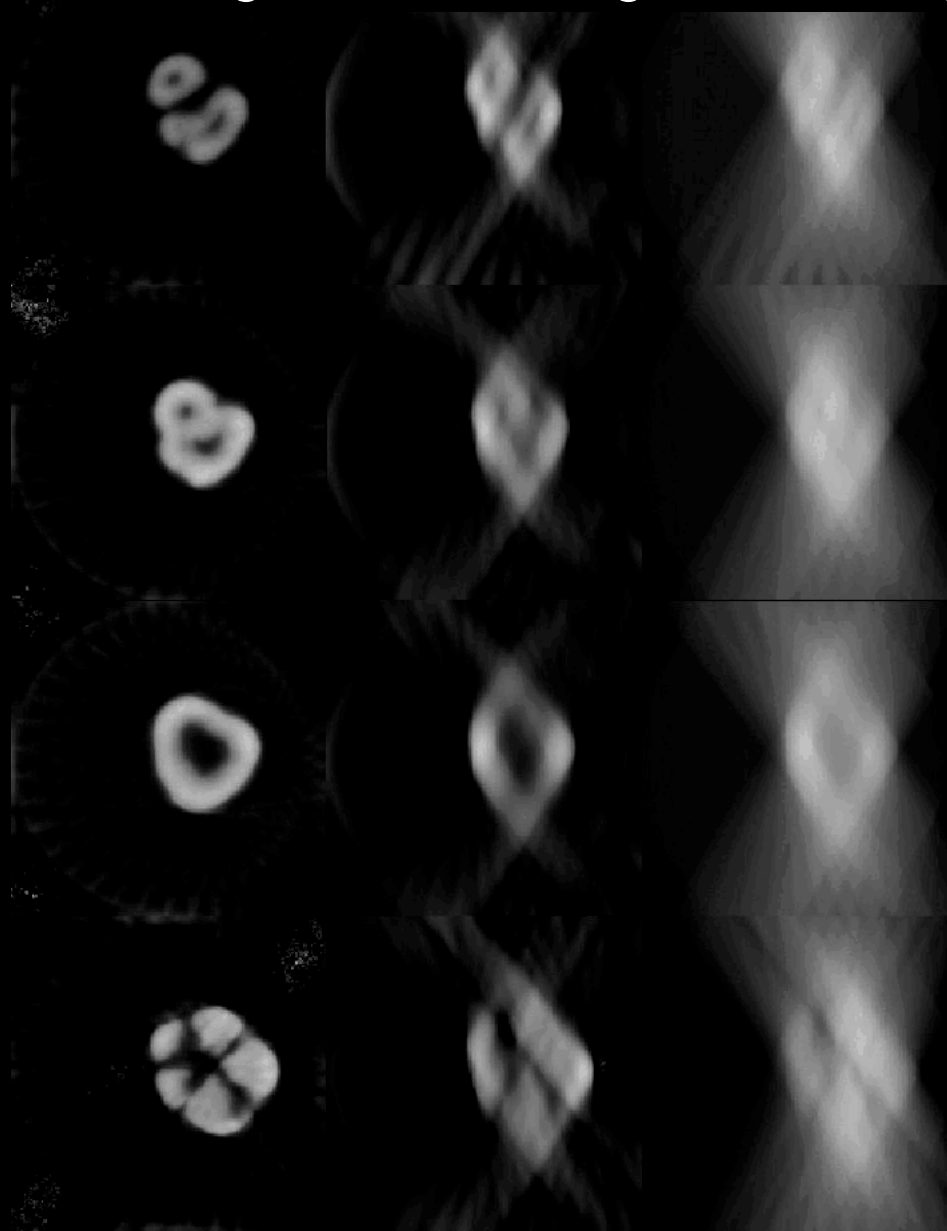
full angle

**Bayes**

limited angle

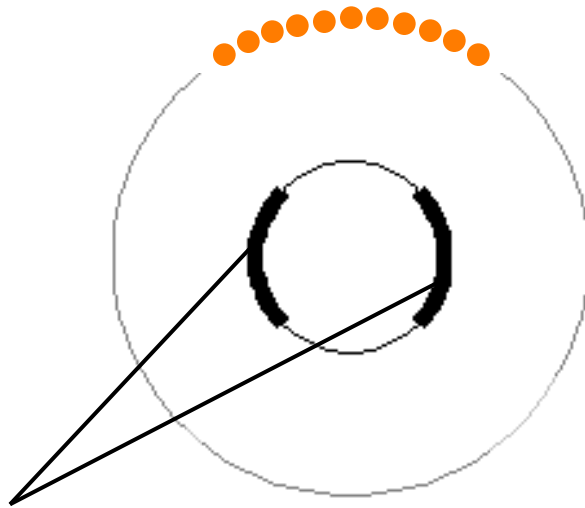
**tomo**

limited angle

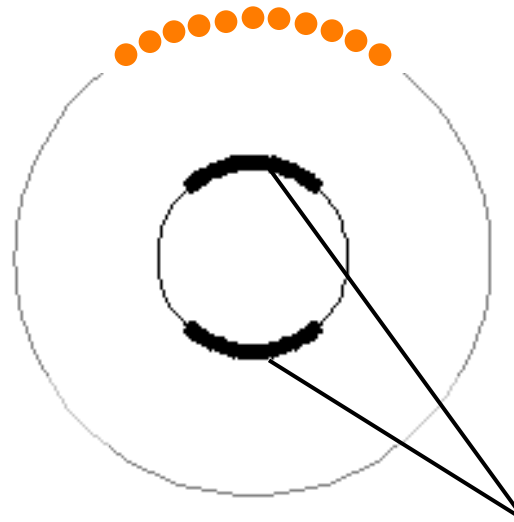


# Some parts of the boundary are strongly visible in projection data

X-ray source locations



visible parts  
of boundary



indetectable parts  
of boundary

Microlocal analysis of recoverable singularities is available in **Greenleaf & Uhlmann** (1989), **Quinto** (1993) and **Ramm & Katsevich** (1996), based on earlier work by Guillemin.

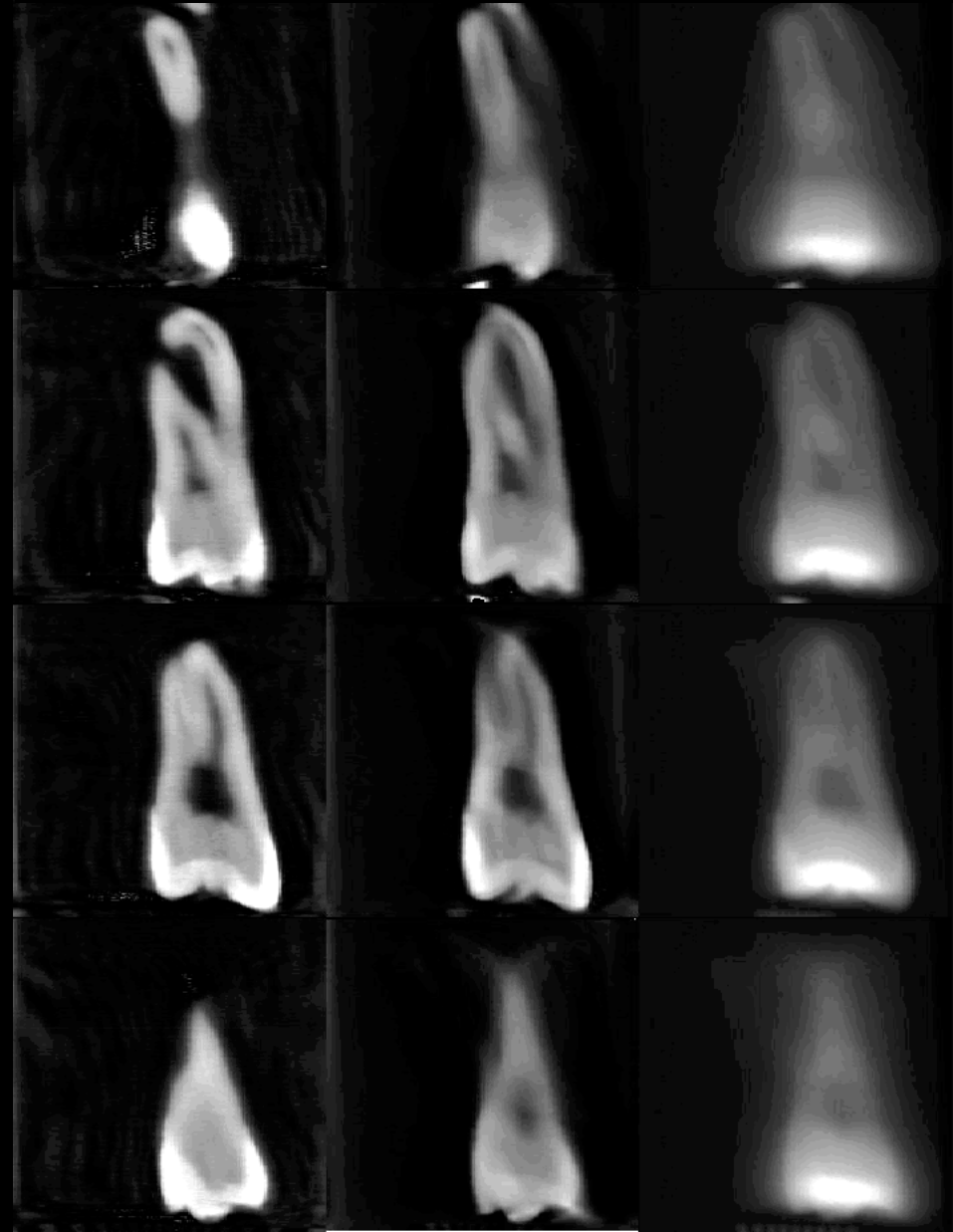


# Vertical slices:

**truth**  
full angle

**Bayes**  
limited angle

**tomo**  
limited angle

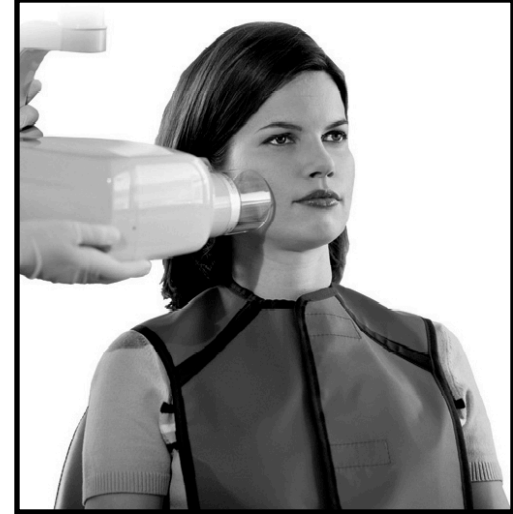


Kolehmainen, S,  
Järvenpää, Kaipio,  
Koistinen, Lassas,  
Pirttilä, Somersalo  
(2003)

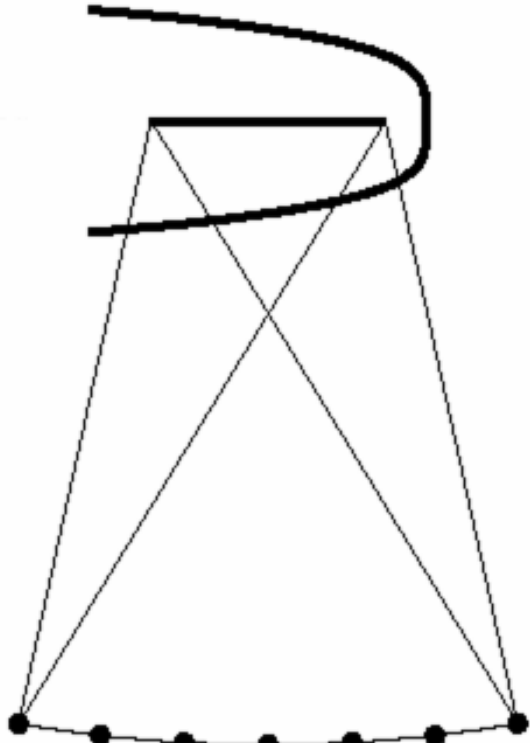
After 11 hours of laboratory work



# Experimental setup for chairside 3D imaging models the clinical situation



# Details of this limited angle experiment



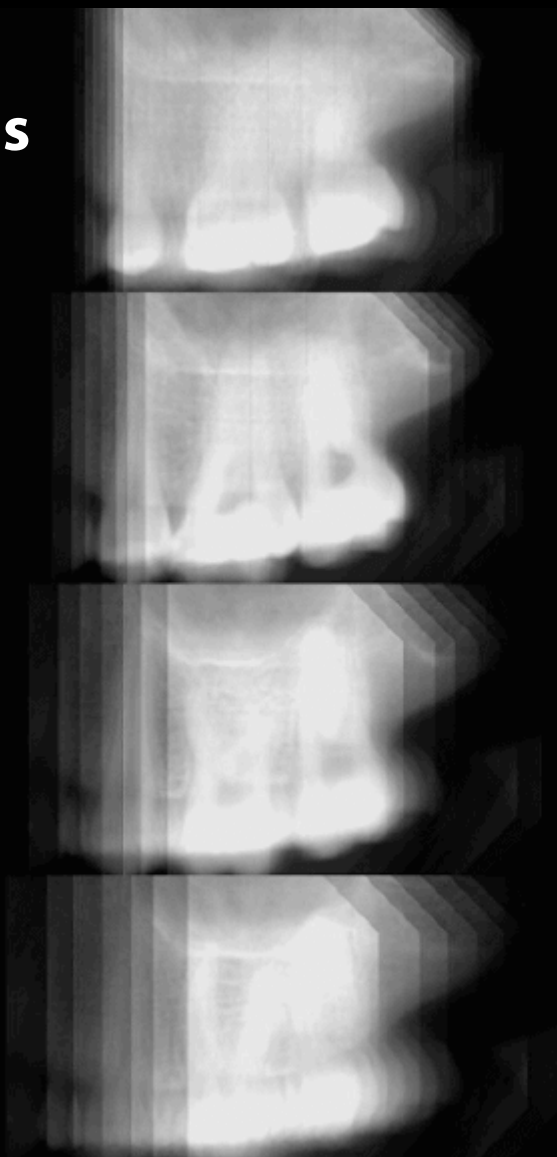
Opening angle 60 degrees

Seven digital intraoral  
radiographs  
(664 x 872 pixels each)

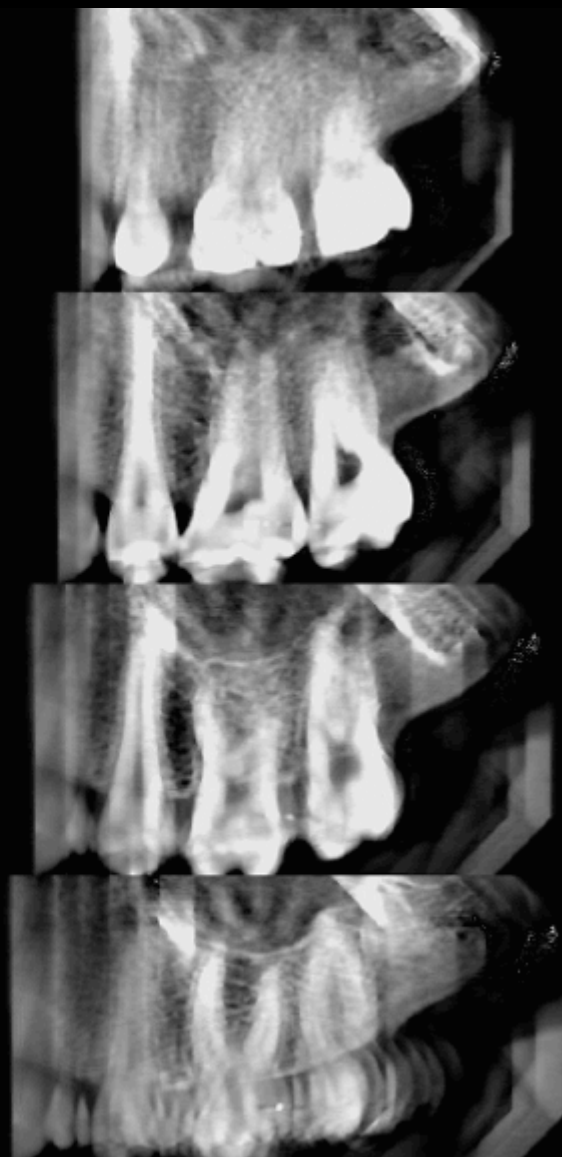


There are 42 496 000 unknowns and 4 053 056 linear equations.  
Computation is divided into 400 approximately 2D problems.

**Tomo-  
synthesis**



**Bayes-MAP**



S, Kolehmainen, Järvenpää, Kaipio, Koistinen, Lassas, Pirttilä and Somersalo 2003

# Data from a knee phantom using a surgical C-arm X-ray device, reconstruction by level set method



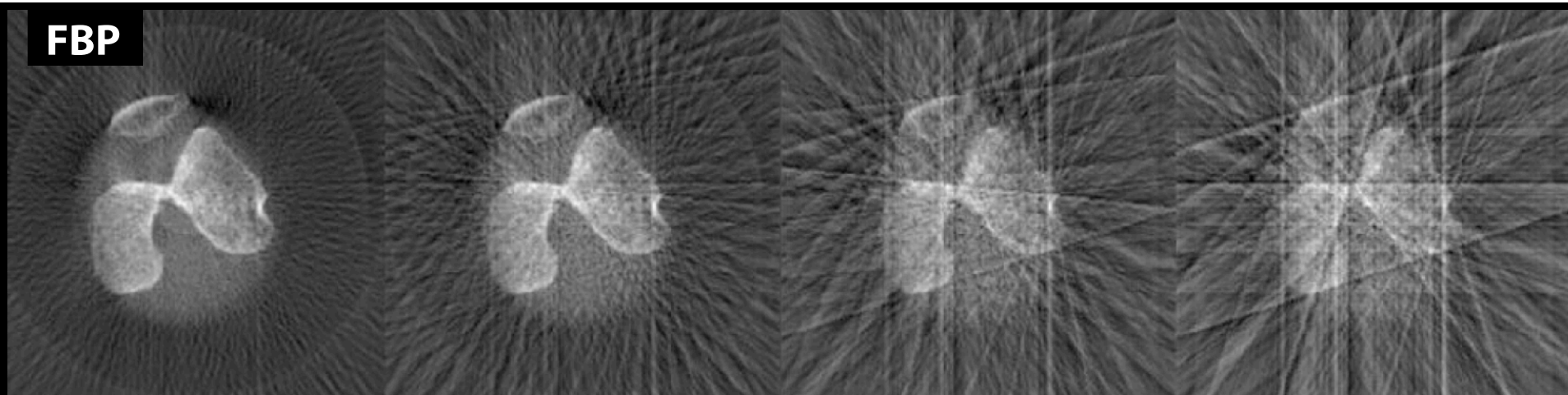
60 projections

40 projections

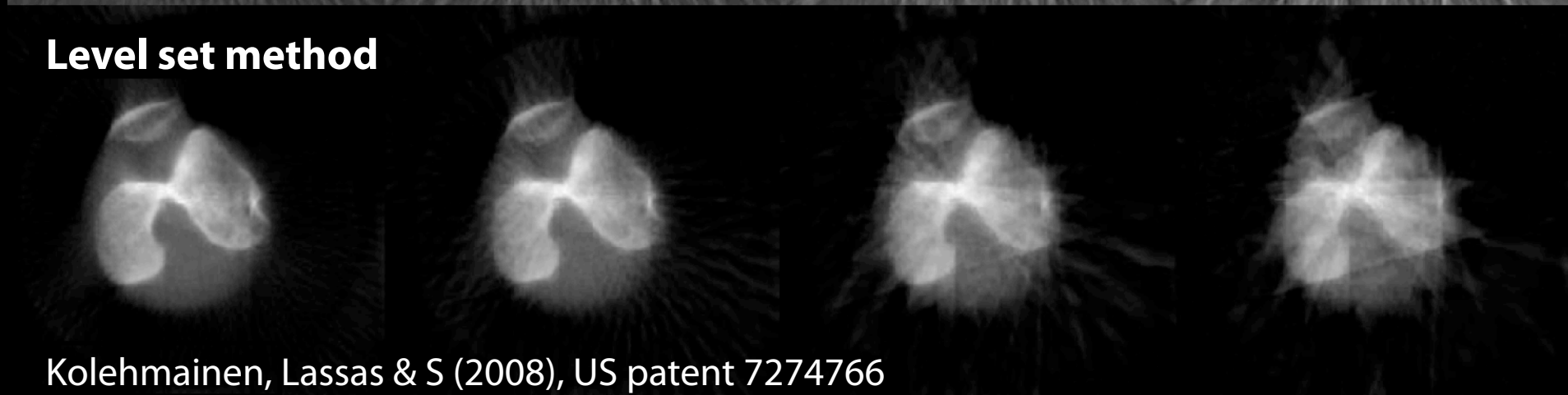
20 projections

10 projections

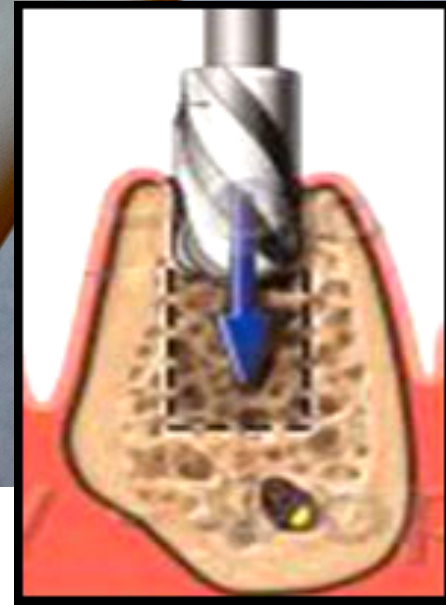
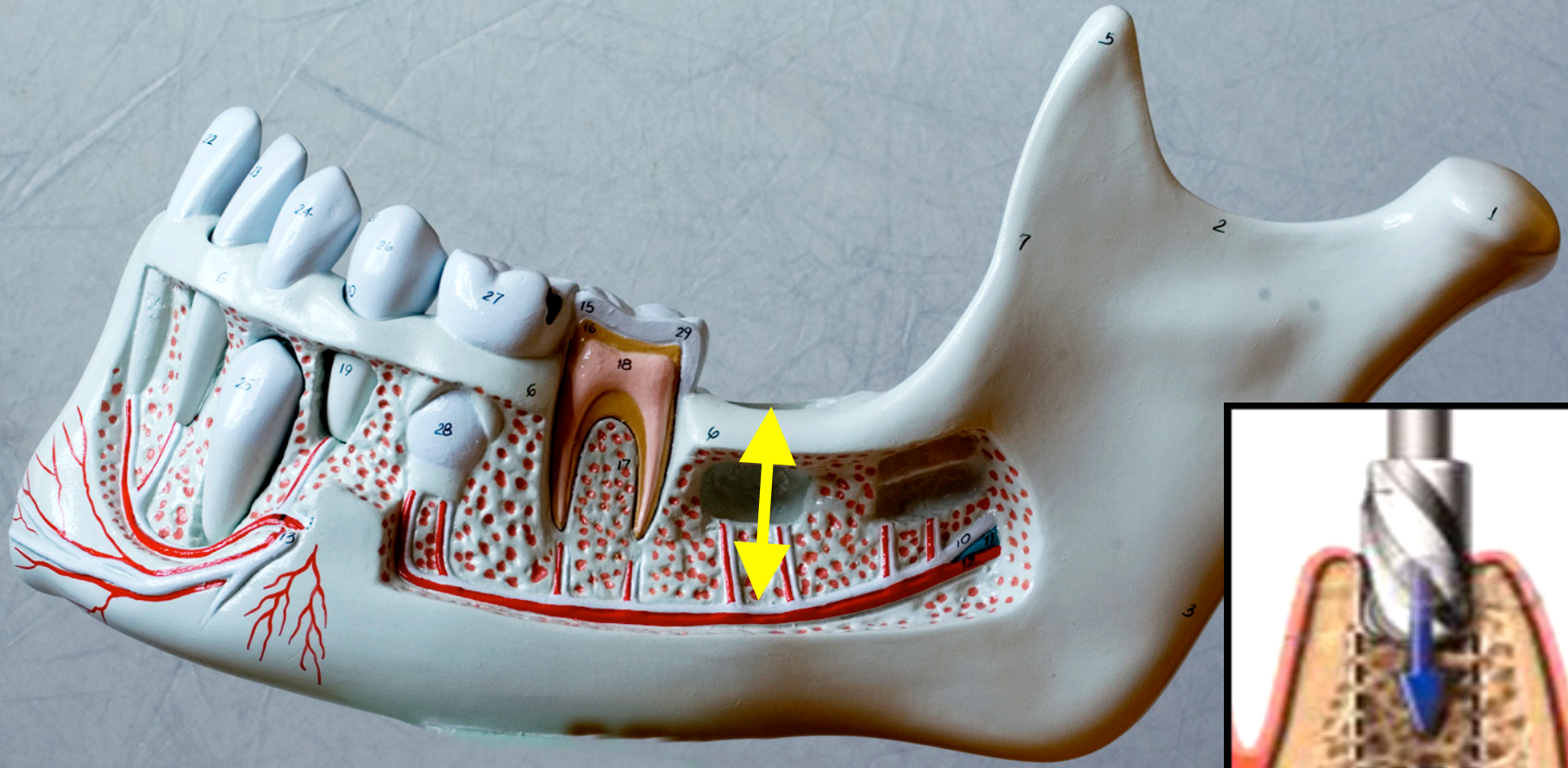
**FBP**



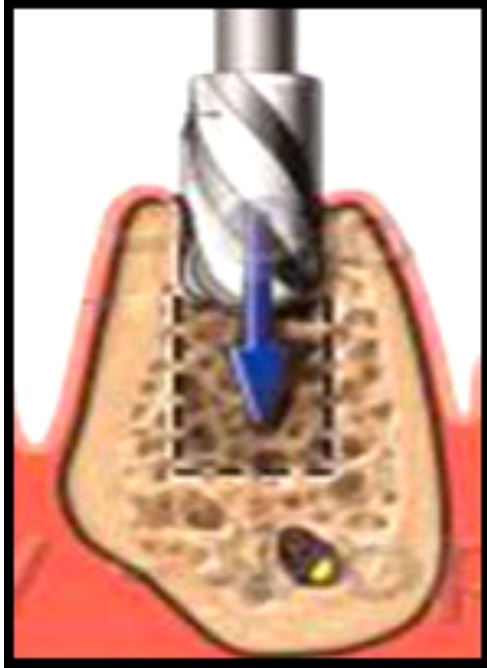
**Level set method**



# Application: dental implant planning, where a missing tooth is replaced by an implant



# Three-dimensional information is crucial for dental implant planning



The hole must be drilled deep enough for sturdy attachment but not so deep that the mandibular nerve is damaged.

Two-dimensional X-ray projection images are not suitable for assessing the proper depth because of geometric distortion.

Three-dimensional reconstruction of the tissue is needed, but a traditional CT scan is not practical due to high cost, too low resolution and too high radiation dose.

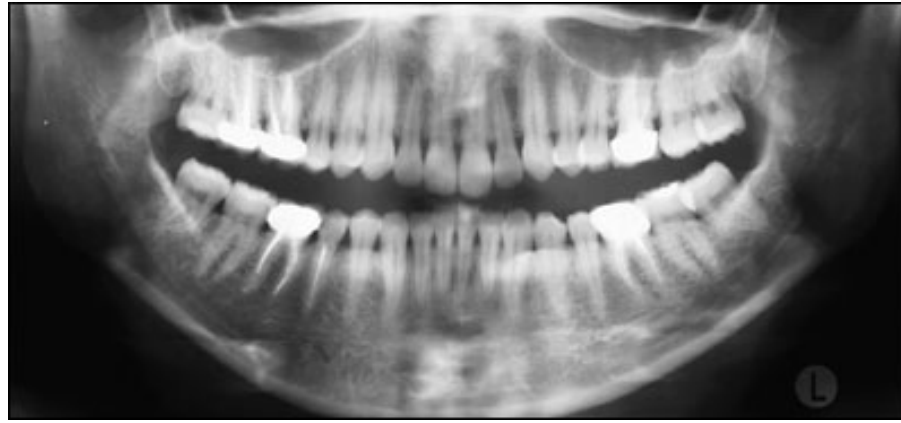


Low-dose 3D X-ray imaging is an ideal solution: it is based on a small number of X-ray projection images recorded with a cost-effective device.



# Panoramic X-ray device rotates around the head and produces a general picture of teeth

Panoramic imaging was invented by Yrjö Paatero in 1950's.

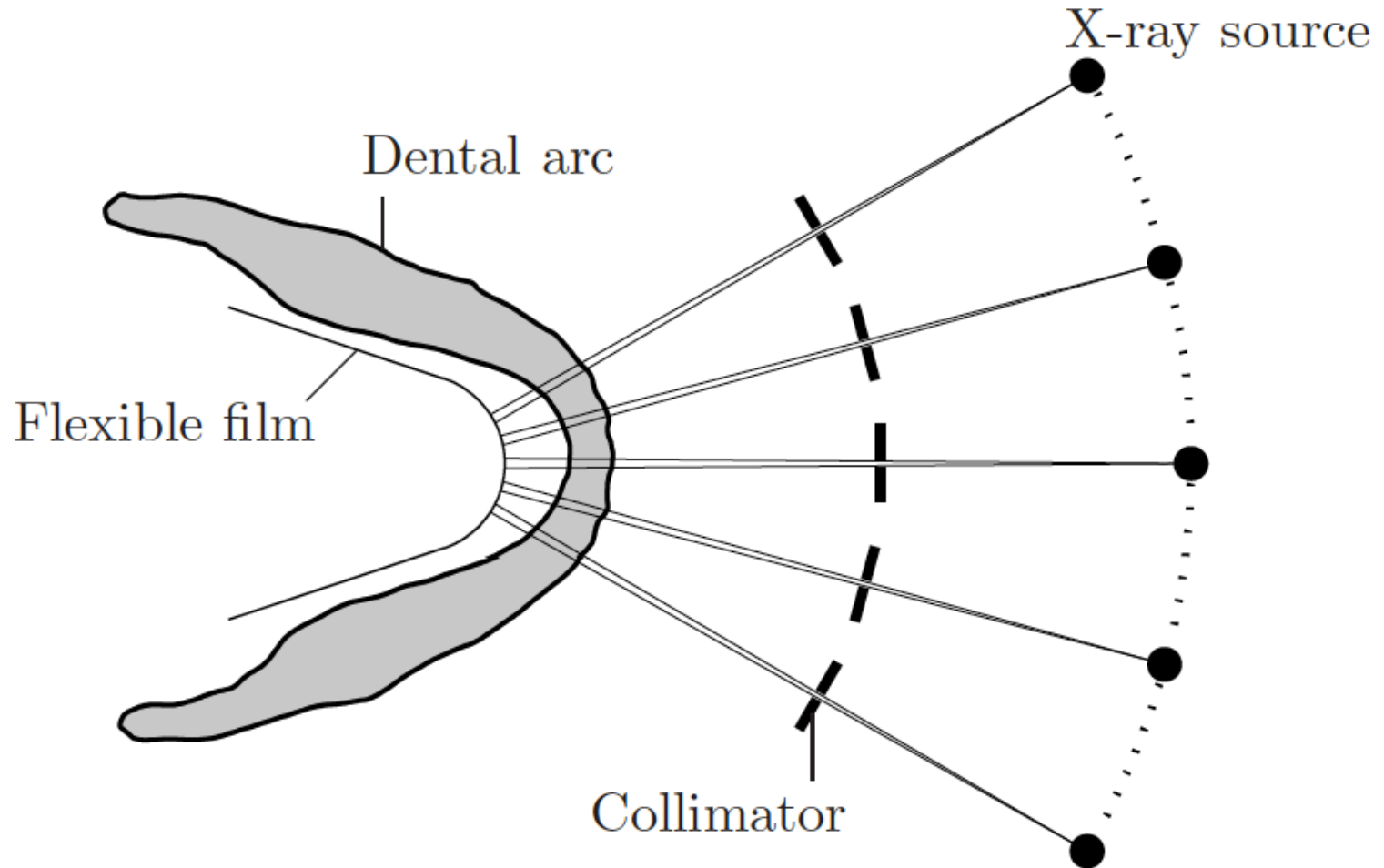


Nowadays a panoramic device is standard equipment at every dental clinic around the world.

In our project, we reprogrammed the device so that it collects limited-angle data.



# Early approach for all-teeth X-ray imaging pioneered by Hisatugu Numata in 1933



# This is the principle of panoramic X-ray imaging

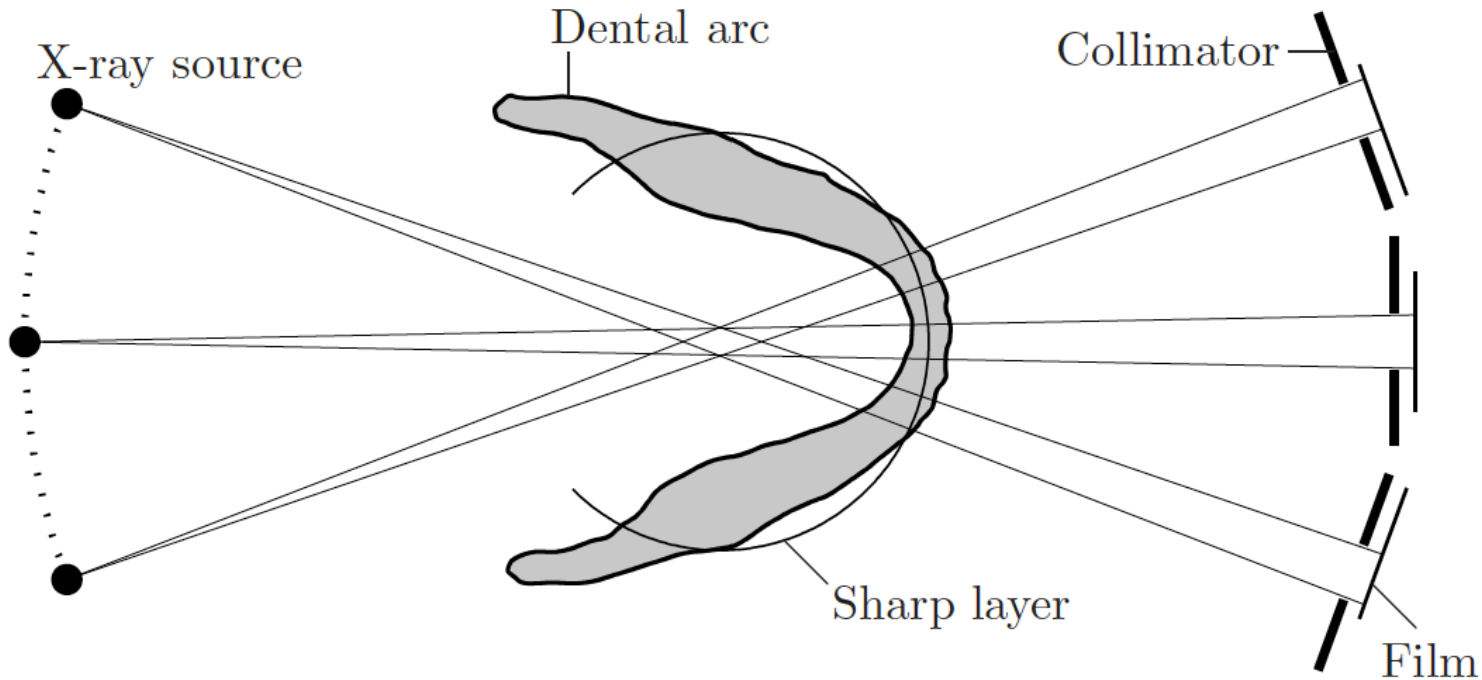


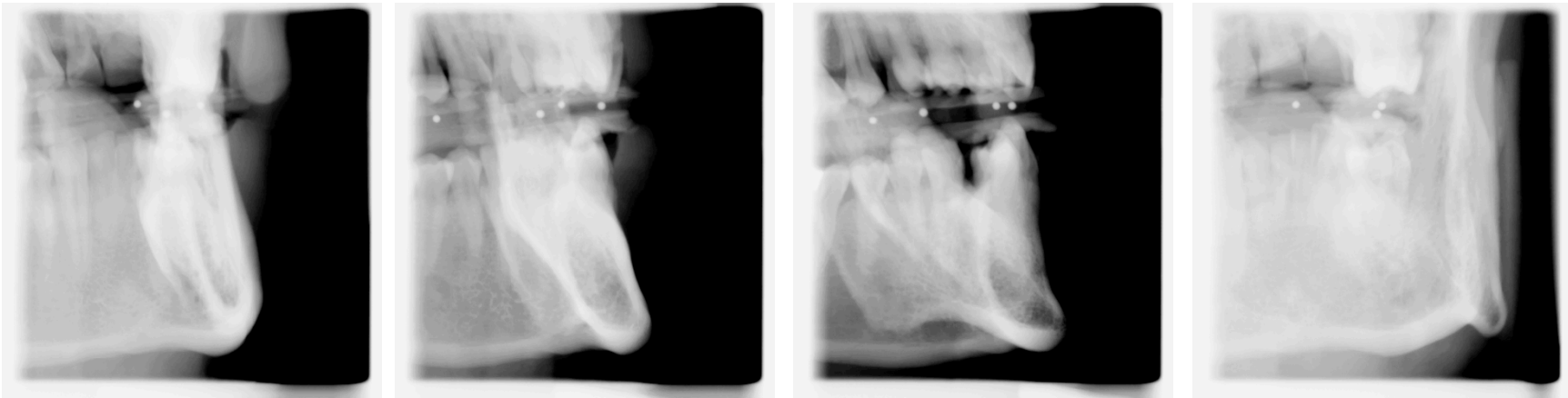
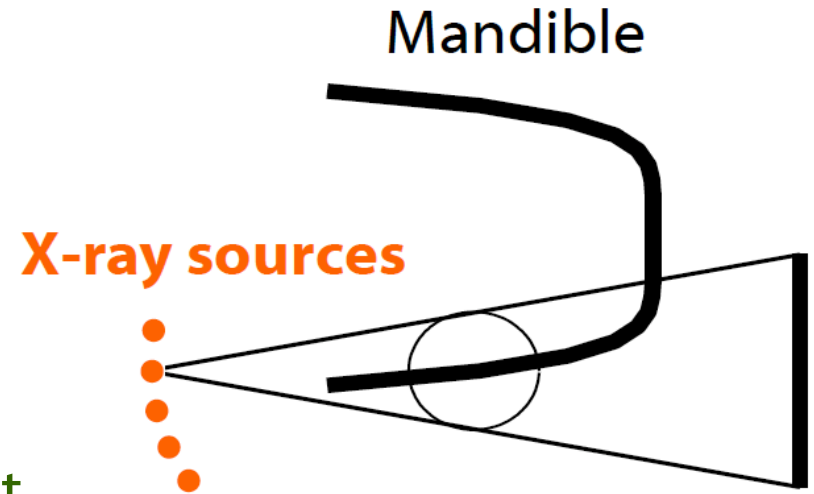
Figure 9.10: Principle of film-based extraoral (film outside the mouth) panoramic dental X-ray imaging, shown in a simplified cylindrical geometry and exaggerated angles for clarity. Note the crucial linear movement of the film with respect to the collimator slit. Due to the simplified geometry, the sharp layer does not follow the dental arc properly. In practice this problem is solved by varying the linear speed of the film and moving the center of rotation during the exposure.

# We reprogram the panoramic X-ray device so that it collects projection data by scanning

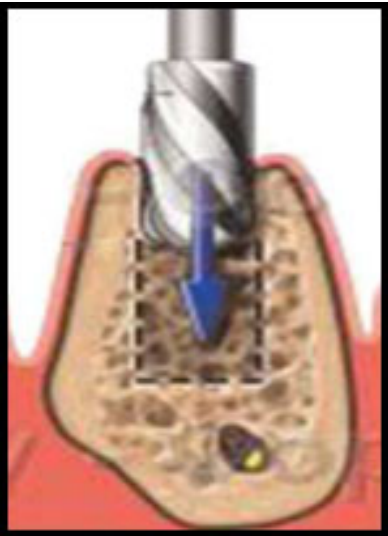
**11** projection images of the mandibular area

**40** degrees angle of view

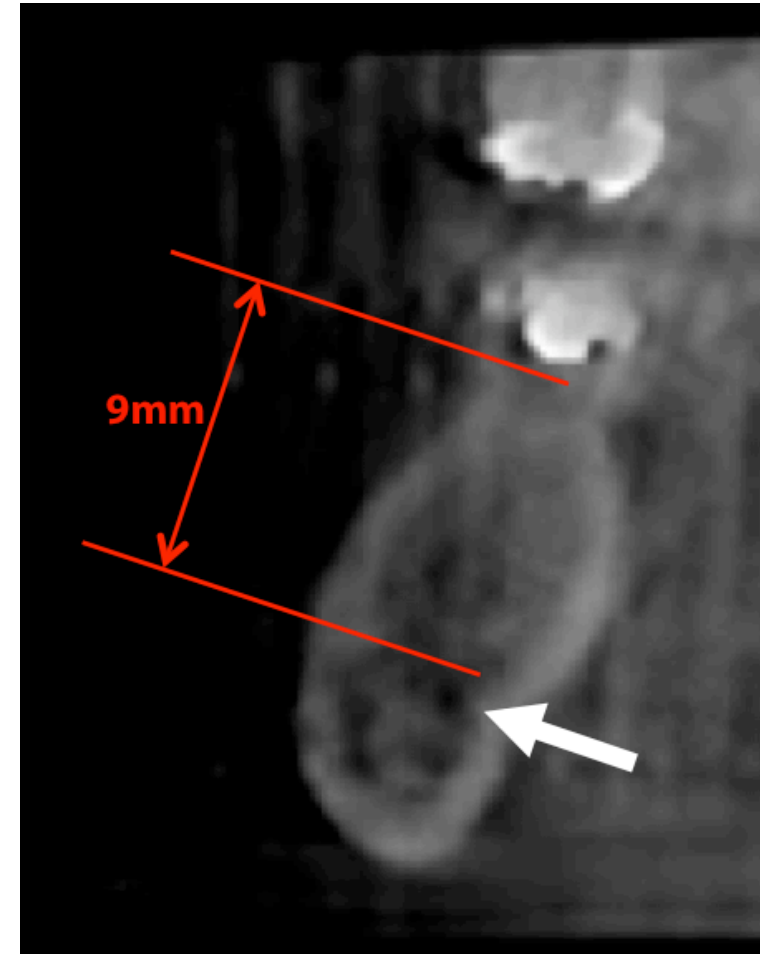
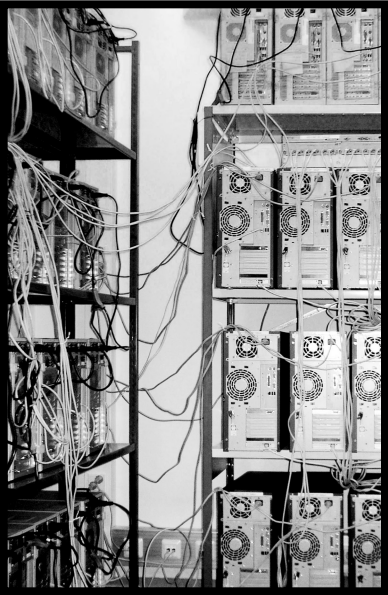
**1000 x 1000** pixels per image, formed by a scanning movement



# Limited angle Bayesian reconstruction can be used for locating the mandibular nerve



**7 200 000 unknowns,**  
**2 100 000 data points.**  
Parallel processing with a  
13-node Beowulf cluster  
and GPGPU computing  
yields computation time  
less than 4 minutes.



Cederlund, Kalke & Welander (2009)  
Kolehmainen, Lassas & S (2008)  
Kolehmainen, Vanne, S, Järvenpää, Kaipio, Lassas & Kalke (2006)  
United States patent 7269241

# The Bayesian low-dose imaging technique has been commercialized by Palodex Group

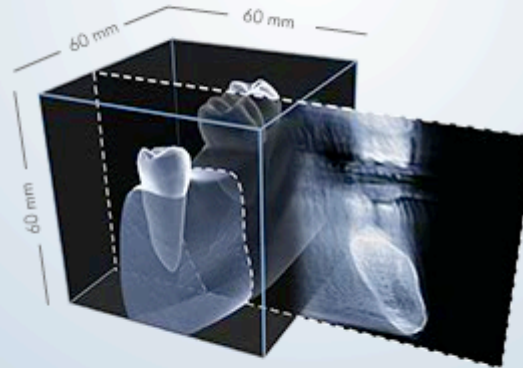
The **VT device** has been in the market from year 2007; thousands of units sold. See **[www.vt-cube.com](http://www.vt-cube.com)**.

It is remarkable that an existing 2D X-ray imaging product (panoramic device) becomes a 3D imaging product by a software update.

The core of that update is a mathematical inversion algorithm.

## VT — essential information for implantology

**VT option** is a Narrow Beam Volumetric Tomography (NBVT) imaging tool that provides digital tomography with reliable measurements and excellent image quality for implant site evaluation.



### What does VT do?

One VT image covers a cubical area of ~ 60 mm per side, producing 256 cross-sectional slices with a minimum slice thickness of 0.23 mm.

### How does VT do this?

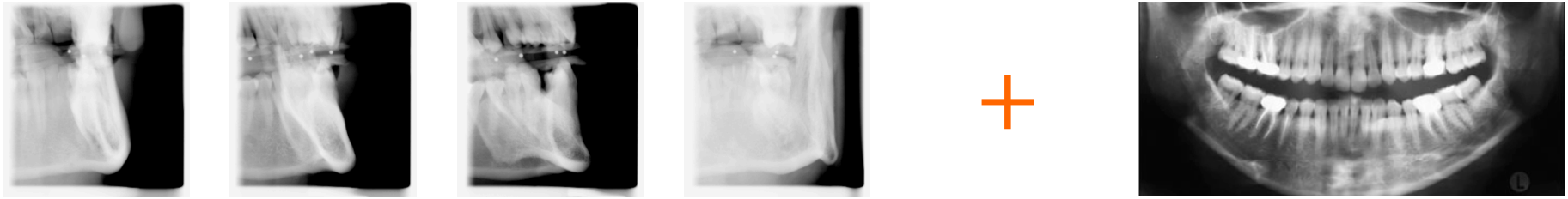
The resulting 3D model is reconstructed from a set of projection images targeted only on the region of interest. The reconstructed, wide volumetric view offers 256 slices, from which the optimal slice or any number of slices can be viewed.

# The radiation dose of the VT device is the lowest among 3D dental imaging modalities

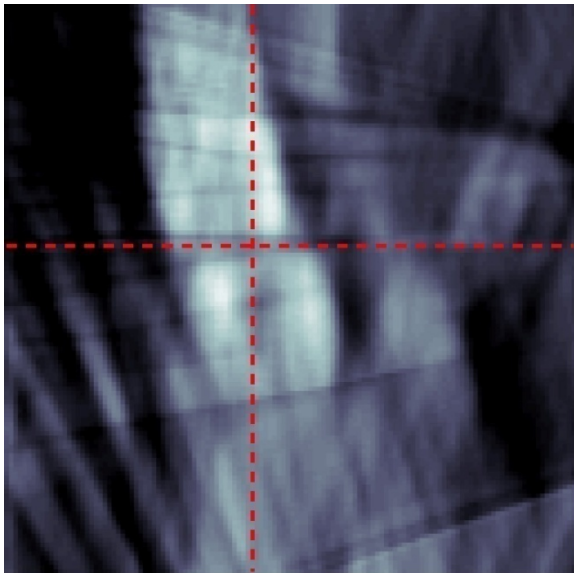
<b>Modality</b>	<b><math>\mu\text{Sv}</math></b>
Head CT	2100
CB Mercuray	558
i-Cat	193
NewTom 3G	59
<b>VT device</b>	<b>12</b>
Panoramic image (2D)	6

Ludlow et al, *Dentomaxillofacial Radiology* (2006) 35, 219–226

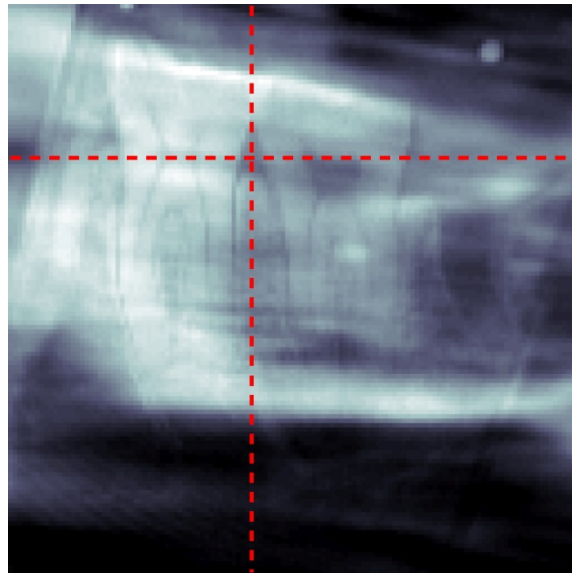
# The use of a panoramic device for 3D imaging is enhanced by including panoramic data



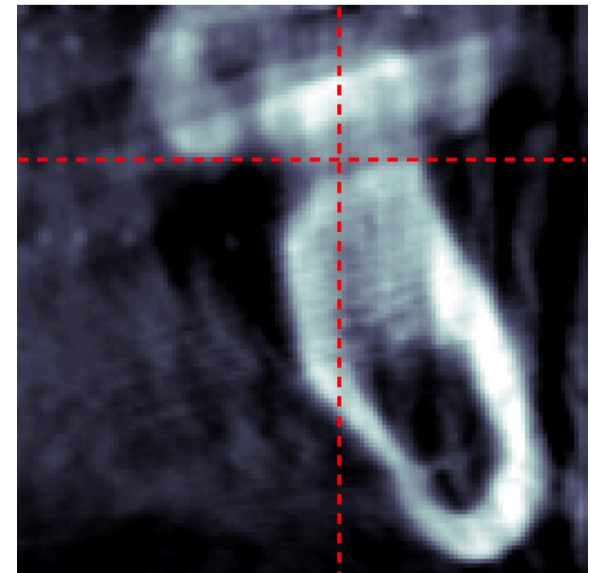
Navigation image



Navigation image

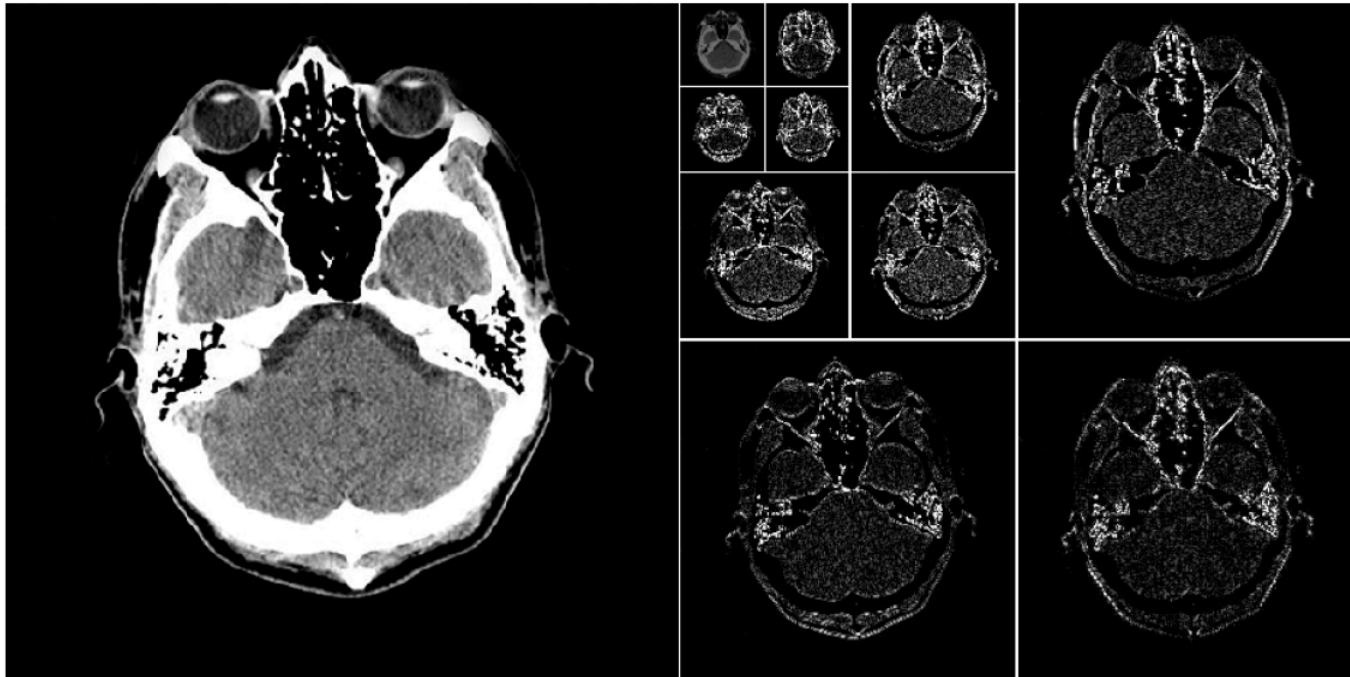


Measure here

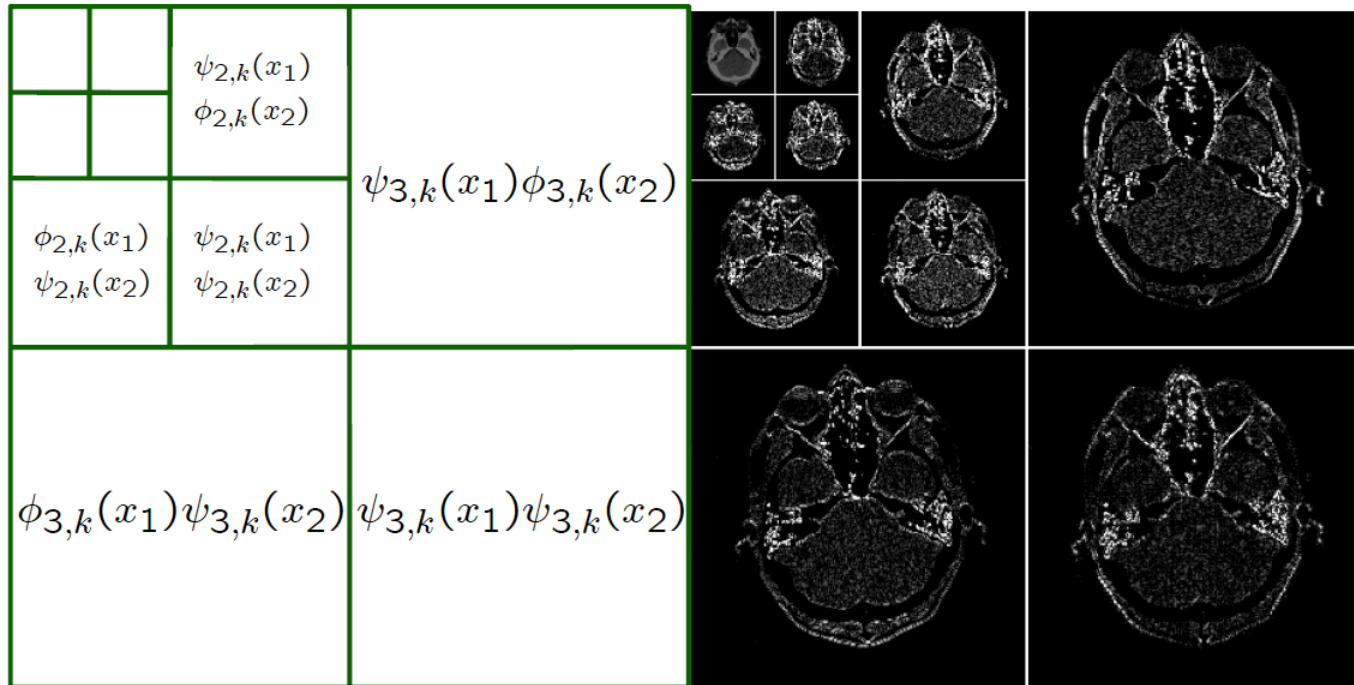




# Wavelet transform divides a function into details at different scales



# We introduce a convenient renumbering of the basis functions



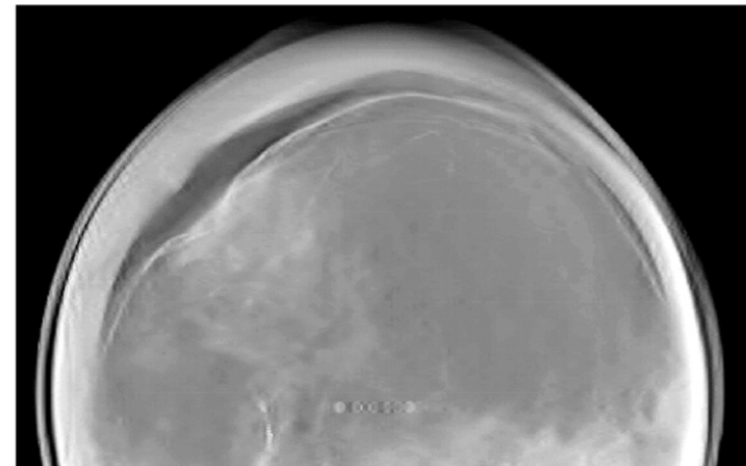
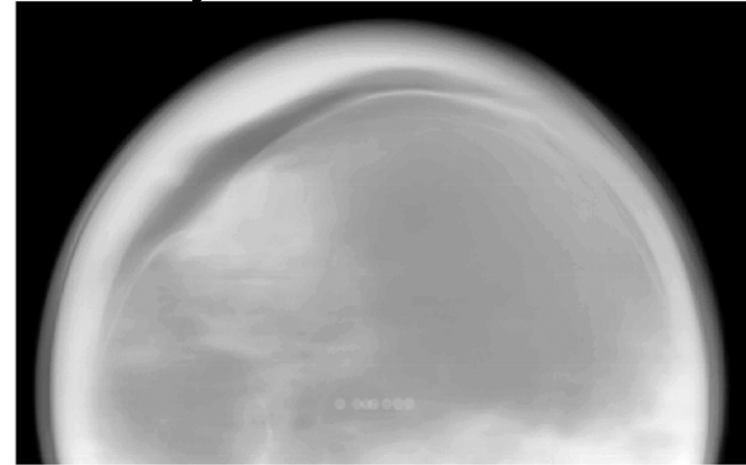
$$f(x) = \sum_{\ell=1}^{\infty} c_{\ell} \psi_{\ell}(x)$$

# Limited angle tomography results for X-ray mammography



Rantala *et al.* (2006)  
US patent 7215730

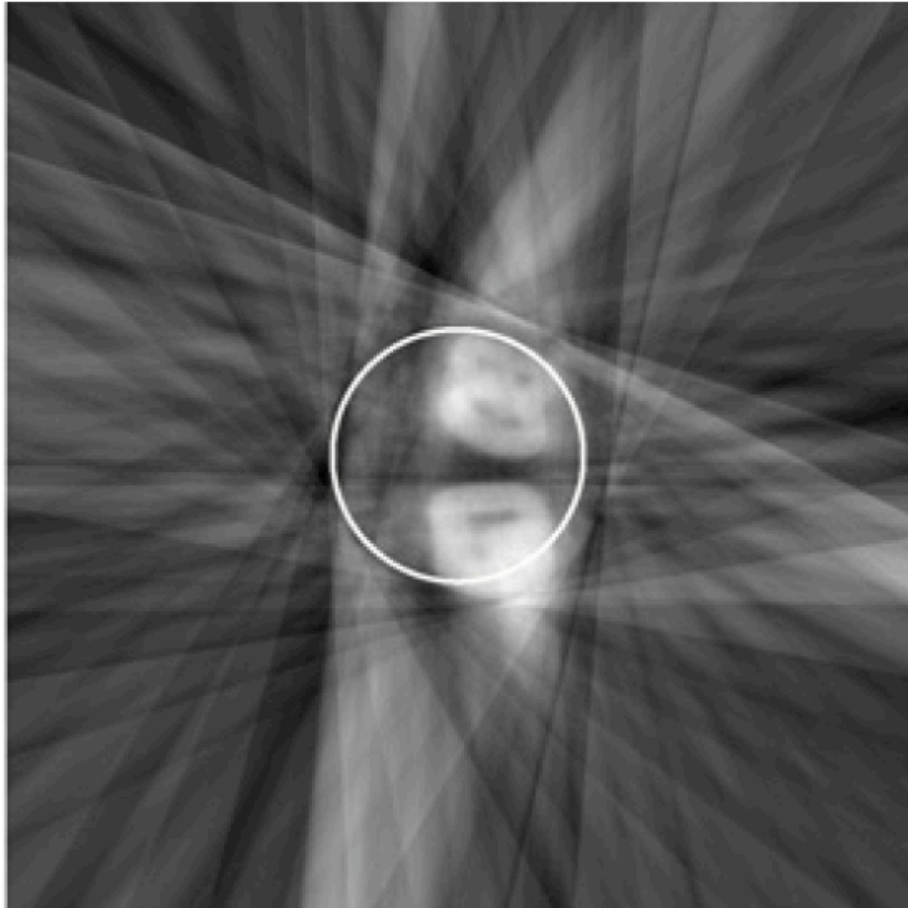
Tomosynthesis



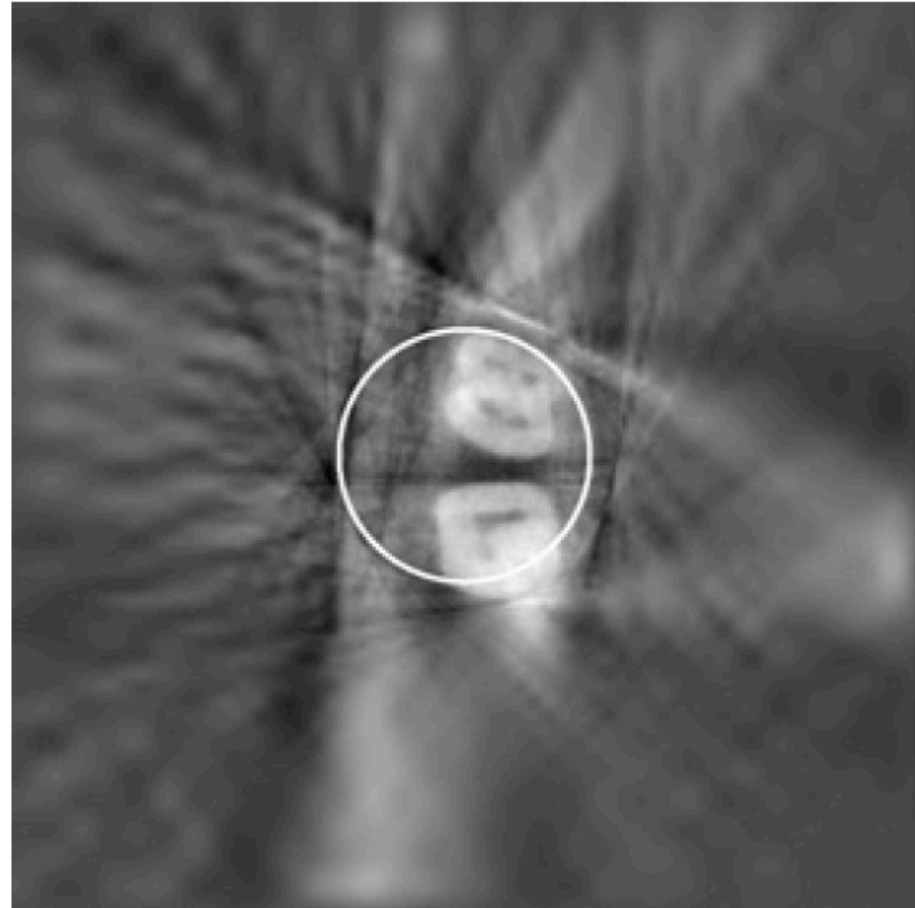
MAP estimate, Besov prior,  
 $p=1.5=q$  and  $s=0.5$

# Local tomography results for dental X-ray imaging; data from dry mandible (jawbone)

All 6 wavelet scales outside ROI



Only coarsest wavelets outside ROI

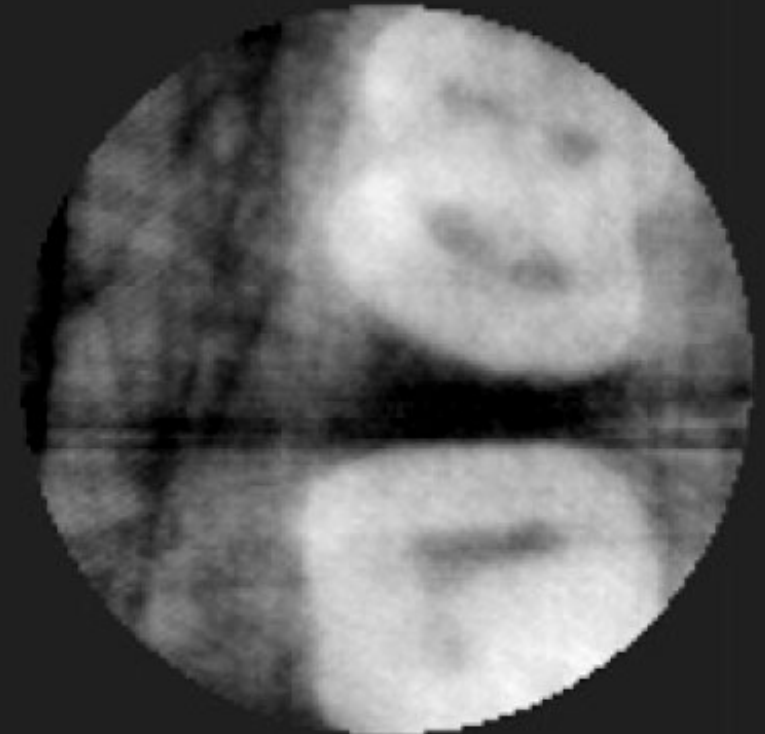


# Comparison of our local tomography results with Lambda-tomography

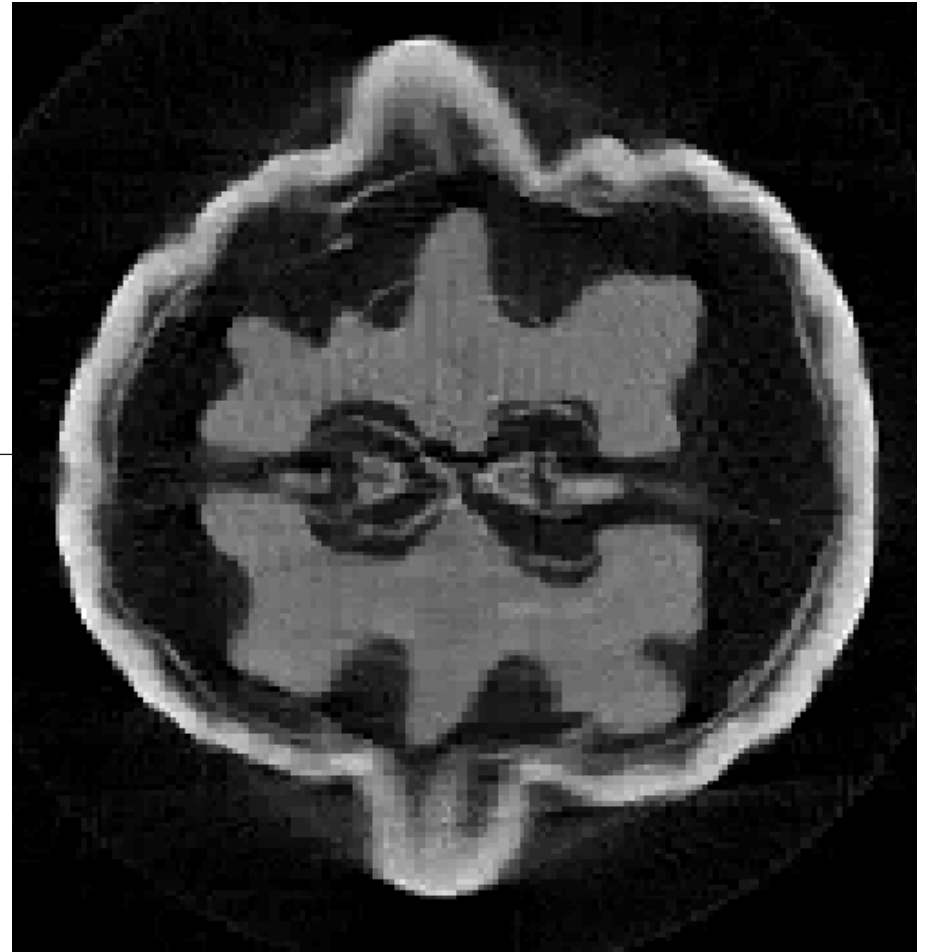
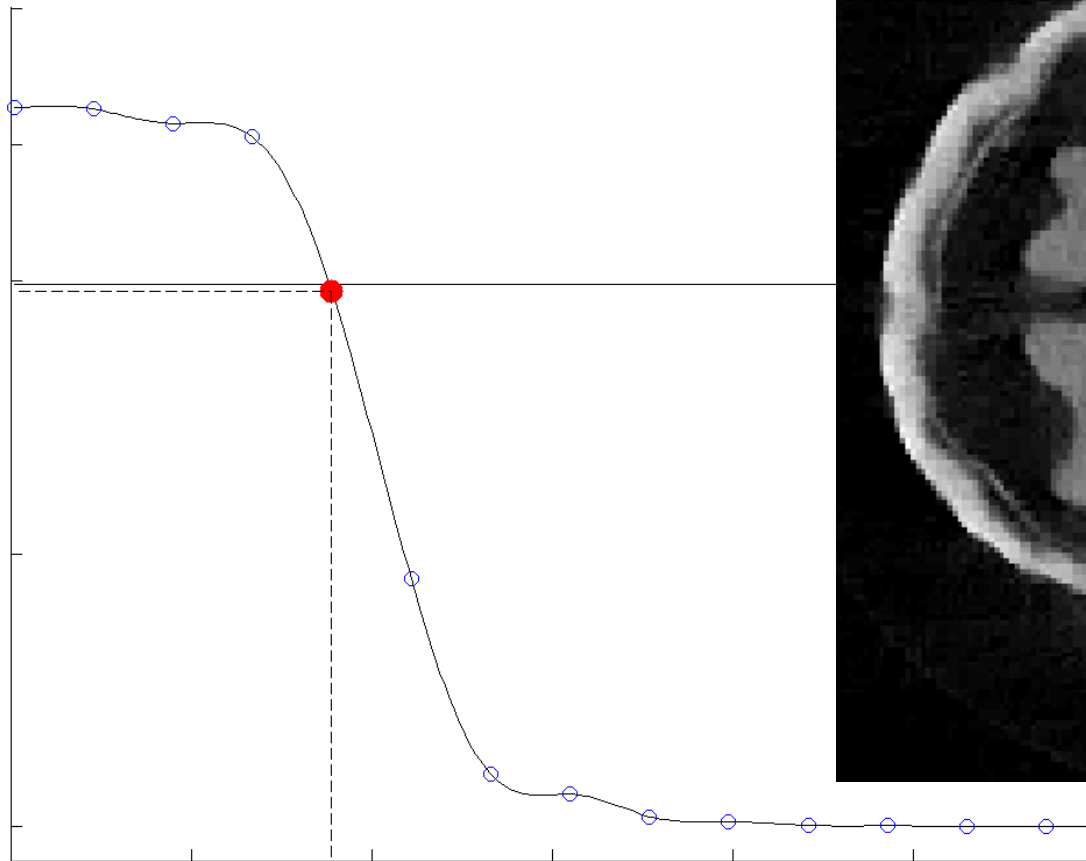
Lambda-tomography



Besov prior,  $p=q=1.5$  and  $s=0.5$



# This is a preliminary example of X-ray tomography using the B111 prior



# Combining several source-detector pairs enables 4-dimensional X-ray imaging

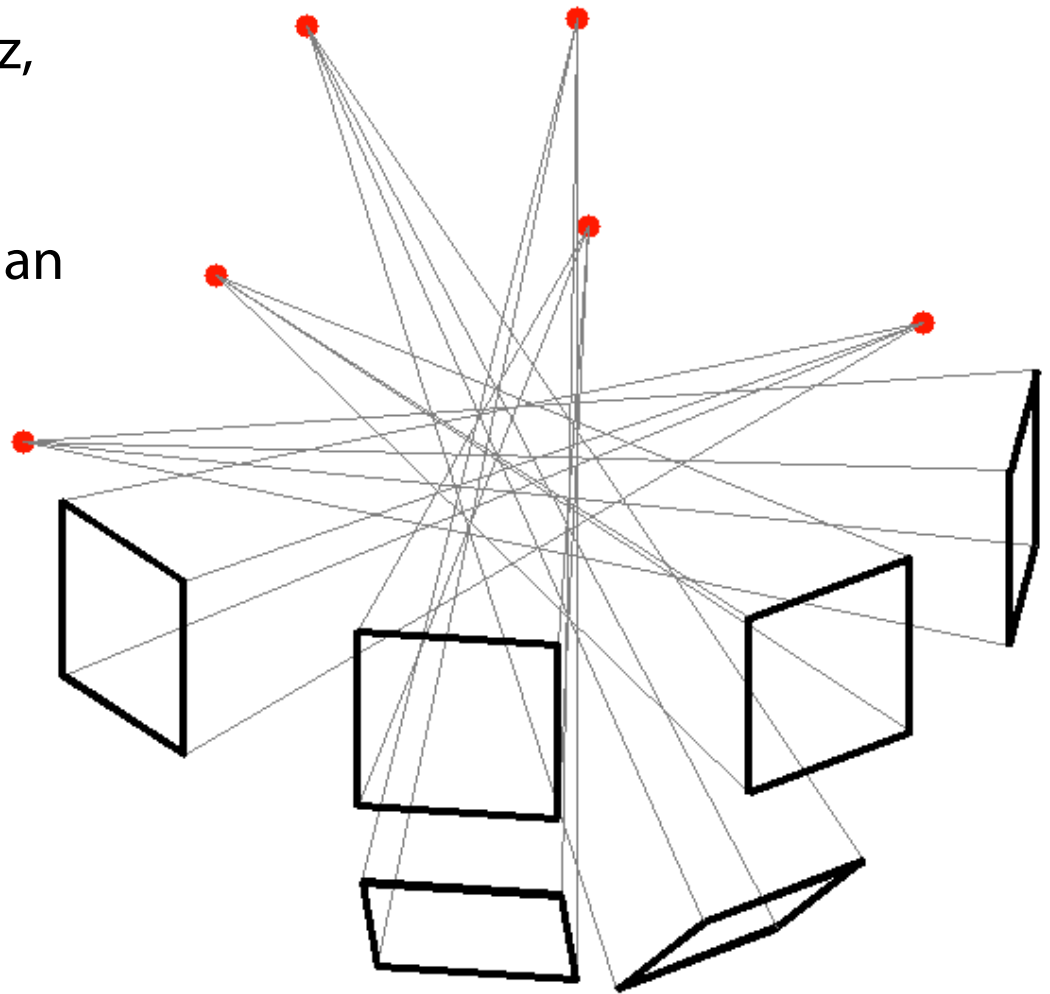
X-ray detectors are available with frame rates up to 200 Hz, providing dynamic data.

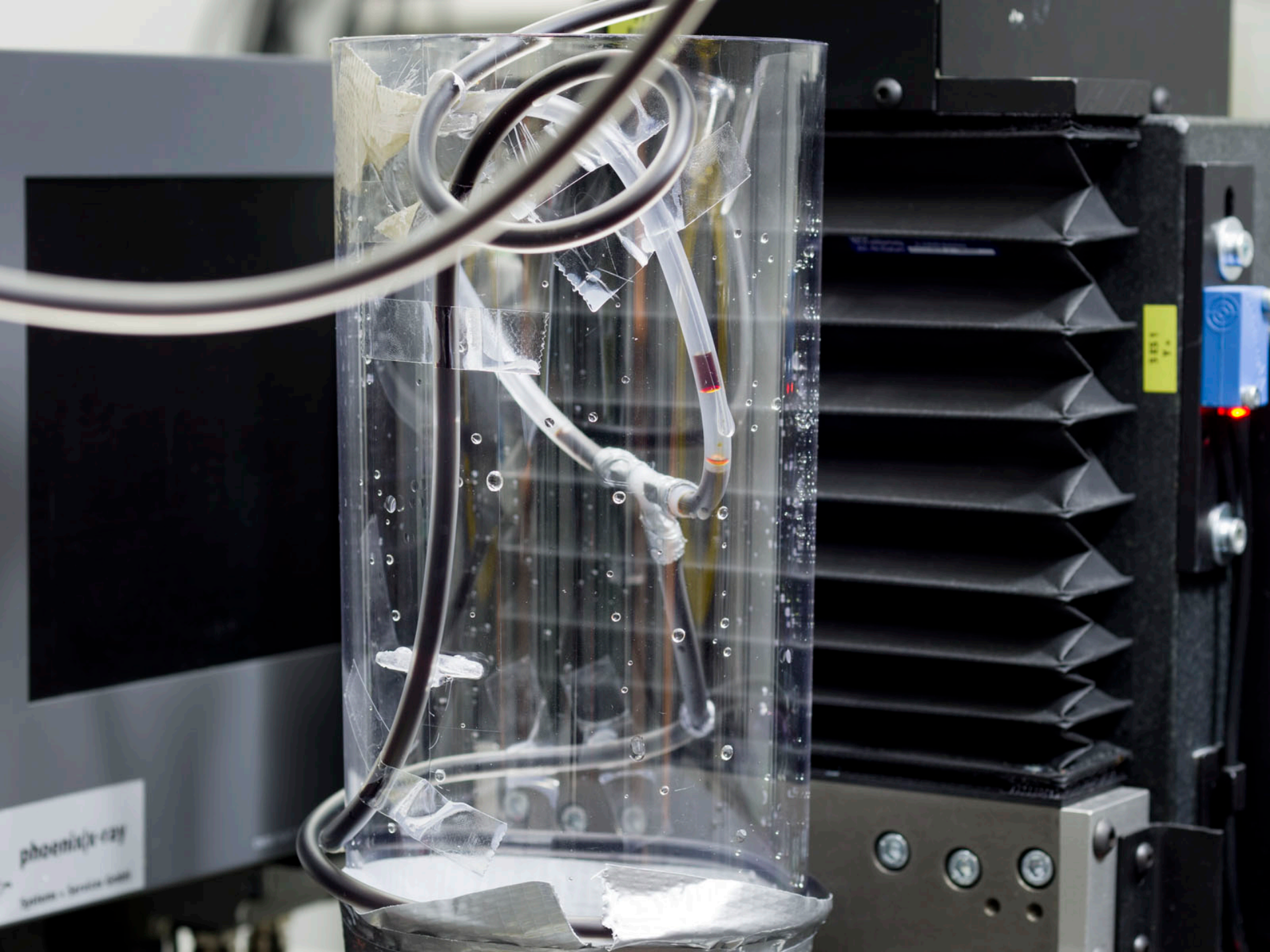
We can compute a 3D Bayesian estimate for each time; there are no moving parts.

Applications include

- cardiac imaging
- angiography**
- dental cone-beam imaging
- veterinary medicine
- non-destructive testing

Patent pending





phoenix/x-ray

System - Service Unit

1351  
1.2



